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(54) Title: METHOD OF ESTABLISHING THE OPTIMAL RADIATION DOSE FOR RADIOPHARMACEUTICAL TREATMENT OF DISEASE

(57) Abstract

A method for determining the number of millicuries to be administered to a patient so as to deliver a given centigray (cGy) dose to either the patient's lean body or the patient's total body. The method includes the steps of injecting a radioactive tracer into a patient, determining radiation levels in the whole body, calculating a geometric mean based on the radiation levels, determining the percent-injected activity remaining in the body at each time point, plotting the percent-injected activity versus calculated time from infusion on a log-linear graph, determining the effective half-life and the rate of clearance from the log-linear graph, cross-indexing the effective half-life value with the patient's body weight, and multiplying the determined amount of therapeutic millicuries per centigray by the amount of desired centigray to be administered.

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At present, the radiopharmaceutical is commonly introduced into the blood for ultimate internal distribution through conventionally known methods such as through intravenous, inhalation, or oral administration. A common unit of radioactivity is the millicurie, or mCi.

5 The general difficulty of the administration of radiopharmaceuticals for therapy lies in the fact that if the patient is given too much radioactivity, toxicity results. On the other hand, it is necessary to give enough of the radiopharmaceutical so that the disease is successfully treated. The most common specific side effect of radiopharmaceutical treatment is bone marrow suppression or ablation. This is caused by the targeting of the radiopharmaceutical (or the radiolabel) to the bone or bone marrow or is due to circulation of the radioantibody through the blood vessels (including the marrow). In general, this situation could lead to bleeding, infection or death. This side effect (as well as other undesirable side effects) is caused by the inaccuracy of known methods used to determine the radioactive dose for the individual patient. For example, up to a five fold difference in the radiation dose to blood, bone marrow, or body received/mCi of the particular radioantibody administered may exist between patients. (Radiation dose is defined as the total amount of energy per unit mass deposited in an individual as a result of radioactive decay.) These differences are tied to the fact that individuals are physiologically different. Not only are individuals of different sizes and, to some degree, densities, they also differ in abilities to metabolize and clear radiopharmaceuticals. For example, if the radioactivity is attached to a monoclonal antibody, the radioactivity might be eliminated from different patients such that a half life of clearance of radioactivity of three days might be identified in a first patient, while a half life of clearance of radioactivity of six days is identified in a second patient.

20 Accordingly, the challenge facing the physician today is determining the correct number of millicuries to be administered to a particular patient having a particular disease at a particular stage of development of that disease. The number of millicuries to be administered is based on the prescription of a

**METHOD OF ESTABLISHING THE OPTIMAL RADIATION DOSE
FOR RADIOPHARMACEUTICAL TREATMENT OF DISEASE**

BACKGROUND OF THE INVENTION

1. Field of the Invention

The present invention relates to the administration of radiopharmaceutical compounds for the therapy of disease including cancer. More particularly, the present invention relates to a method of establishing the optimal effective radiation dose for treatment of disease, the method minimizing toxicity while preserving therapeutic activity.

2. Description of the Relevant Art

Radiopharmaceuticals are compounds composed of radioactive isotopes often bound to other molecules. These radiopharmaceuticals are used in assessing the presence, outline, size, position, or physiology of individual organs or tissues. More significantly for the present invention, radiopharmaceuticals are commonly used in the treatment of disease. For example, radioactive iodine (I-131) is used to treat thyroid cancer or overactive thyroids (Grave's disease). Of considerable importance is the development of monoclonal antibodies having attached radioactive labels. When combined with antibodies that are relatively specific for a particular diseased tissue, such antigen-specific monoclonal antibodies are able to selectively direct comparatively sizable amounts of radiation to the specific disease site. Such treatments are being applied to the treatment of non-Hodgkin's lymphomas, Hodgkin's lymphomas, Hepatoma, colo-rectal cancer, brain tumors, and many other forms of cancer. In addition, the treatments also have the potential to treat other types of disease, including auto-immune conditions such as, for example, Systemic Lupus and Rheumatoid arthritis. Targeted radiopharmaceutical therapy may be ultimately be found to be broadly applicable to a wide variety of neoplastic and benign diseases.

given radiation dose to the "whole body" of the patient, which is dependent upon several factors, including the patient's size and the rate of disappearance of radioantibody from the body as determined by direct measurements of the biodistribution of a tracer dose (a small, non-therapeutic quantity) of radioactivity using a gamma camera, probe detector system, or other radiation detection system. Using such an approach, a "whole body radiation dose" can be calculated from the tracer doses, which can be used to predict the radiation dose the "whole body" would receive from subsequent radiopharmaceutical therapy and which allows the radiation dose administered to be effective. Initial results with this approach using the anti-B-1 antibody have shown excellent therapeutic efficacy and modest toxicity. Results of clinical studies with this approach are detailed in NEJM 7:329, pp. 459-465, 1993 (Kaminski et al.), J. Nucl. Med. 35(5), 233P, 1994 (Wahl et al.), and J. Nucl. Med. 35(5), 101P, 1994 (Wahl et al.).

While this approach to calculating "whole body" radiation dose represents a major improvement over other methods which are not individualized to the patient's individual pharmacology, it still does not fully overcome the difficulties related to the accurate calculation of optimal radiation doses to treat radiosensitive tumors. The inherent failure of this method lies in the fact that the simple assumptions of "whole body" dose are not fully valid in terms of human patient physiology. Accordingly, while radiotoxicity is reduced, it is not fully eliminated or even absolutely minimized. Part of the reason for this failure is that the "whole body" dose approach assumes that a radiopharmaceutical is uniformly distributed throughout the body. There is an assumption underlying this thinking that the body is uniform, and that distribution of chemicals in the body is likewise uniform. This is not the case, as most radiopharmaceuticals, particularly intact monoclonal antibodies, have very limited accumulation in fat tissue compared to considerably greater accumulation in lean body tissue (including bone marrow).

In an effort to improve the accuracy of radiopharmaceutical mCi dosage, a method has been developed that utilizes a parameter directed to

~~total body dose-lean~~ "TBD-lean" to account for the fact that individuals may be modeled as an outer shell of fat (where little radioantibody or radiopharmaceutical accumulation occurs) which surrounds an active lean body mass, including bone marrow.

5 By appreciating the fact that in man there is a "lean body" within a "fat" outer shell, a formula may be used to estimate what percentage of the person is fat and what percent of the person is lean. Thereafter, the radioactivity is traced as essentially being distributed uniformly and totally through the lean component. By first estimating what fraction of the body is lean and then
10 calculating the radioactivity distribution within a given lean volume, the proper dose of radiopharmaceutical for treatment without undue toxicity can be administered on an individualized, case-by-case basis.

15 While resolving many of the difficulties related to the prescription of effective amounts of radiation doses, the prior art nevertheless may be improved upon.

SUMMARY OF THE PRESENT INVENTION

20 The present invention is directed to methods for determining the number of millicuries of radioactivity to be administered to a patient so as to establish a given centigray (cGy) dose to either the patient's lean body or the patient's total body.

25 According to a general method of the present invention, a parameter directed to "total body dose-lean" (TBD-lean) is utilized to account for the fact that individuals may be modeled as an outer shell of fat (where little radioantibody or radiopharmaceutical accumulation occurs) which surrounds an active lean body mass, including bone marrow. By appreciating the fact that in man there is a "lean body" within a "fat" outer shell, a formula may be used to estimate what percentage of the person is fat and what percent of the person is lean. Thereafter, the radioactivity is traced as essentially being
30 distributed uniformly and totally through the lean component. By first estimating what fraction of the body is lean and then calculating the

radioactivity distribution within a given lean volume, the proper dose of radiopharmaceutical for treatment without undue toxicity can be administered on an individual, case-by-case basis.

According to a modified method of the present invention, the following steps are followed.

Initially the rate of clearance or disappearance of radioactivity from a patient is determined by direct measurement across multiple time points using a radiation detection device (such as a NaI probe or a gamma camera). This step determines changes in the radiation concentration of a particular patient over a given period of time. For example, a series of measurements, commonly seven or eight, are done over a period of a week with the first measurement made immediately following a tracer injection of the radiopharmaceutical. The time in hours is determined from the end of the tracer infusion for each measurement, resulting in a variety of values. Appropriate measurement is made of the amount of radioactive disintegration measured from the front of the patient (anterior measurements) and/or from the back of the patient (posterior measurements).

Based on these readings, a geometric mean is calculated. The geometric means may be based upon daily NaI probe measurements, but may also be based upon anterior and posterior conjugate view gamma camera imaging data or other methods of radiation detection. According to the conjugate view approach, a geometric mean is calculated for each time point by multiplying the anterior and posterior readings and determining the square root of the total figure. This mean represents an average number of counts. The background counts are subtracted for a corrected mean. The percent injected activity remaining in the body for each time point is thereafter determined by dividing the counts at a given time by the counts immediately after the tracer is injected. Thereafter, the percent of injected activity versus the calculated time from infusion is plotted on a log linear graph. With these points established on the log linear graph, a line is drawn to determine the

*accumulated
activity from 25*

*residence
time*

intersection of the best fit line with the 50% injected activity line, thereby determining effective half life, or $T_{1/2}$ -effective.

With $T_{1/2}$ -effective thus established and the patient's body weight known, these values are cross-indexed on either a graph (the "graphical" approach) or on a table (the "tabular" approach) to determine the recommended millicuries per centigray (mCi per cGy) to be administered (activity per unit TBD or TBD-lean). (Both the graphical approach and the numerical approach represents activity per unit for total body dose [TBD] or total body dose-lean [TBD-Lean] as a function of total body or lean body mass and $T_{1/2}$ -effective.) Both the graphical and numerical approaches (and their expressed quantities) are features of the present invention.

MTD The actual amount of therapeutic millicuries is then determined by multiplying the recommended mCi per cGy by the amount of desired centigray to be administered.

While the present invention is described as having application to total body dose and total body dose-lean, the method of the present invention is also applicable to dosimetry to blood, bone marrow, and other organs and tissues such as the lung, the liver, and the kidney.

These and other features of the present invention are best understood from the following specification, drawings and examples.

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 is a graph illustrating the relationship of the fat component of the individual with respect to the lean component of the same individual, thus defining the "lean person within the fat person" theory of the present invention; and

Figure 2 is a graph illustrating the elimination of the radioactive element from the individual over time, with the amount of material being on the Y-axis and time being on the X-axis.

Figure 3 is a blank worksheet onto which are to be entered all necessary intermediate values based upon observations of clearance of the

tracer from the body according to an alternate method of the present invention;

Figure 4 is a curve set on a graph indicating therapeutic activity per unit dose calculated from data acquired on days 0, 3, and 7 versus data acquired on days 0, 1, 2, 3, 4, 5, 6, and 7;

Figure 5 is a blank graph consisting of a log linear graph onto which pertinent elimination values are to be marked at different intervals of time;

Figure 6 is similar to the graph of Figure 4 but illustrating two series of elimination values for two sample patients;

Figure 7 is a fused image of a cross-sectional view of the central body compartment of a sample patient following administration of radiolabelled antibodies;

Figure 8 is a graph illustrating the relationship of the fat component of the individual with respect to the lean component of the same individual;

Figures 9a - 9p define a series of graphs used for determining the therapeutic mCi/cGy to be administered based on known $T_{1/2}$ -effective and the patient's mass (in Kg), total body mass (in Kg) for TBD, and lean body mass (in Kg) for TBD-Lean;

Figures 10a - 10h define a series of tables used for determining the therapeutic mCi/cGy to be administered based on known $T_{1/2}$ -effective and the patient's mass (in Kg), total body mass (in Kg) for TBD, and lean body mass (in Kg) for TBD-Lean;

Figure 11 is a three-dimensional graph based on the series of graphs of Figures 9a - 9p;

Figure 12 is chart summarizing the input and output data of twenty-one sample patients;

Figure 13 is a toxicity versus mCi/Kg graph with the data points of the twenty-one sample patients of Figure 12;

Figure 14 is a toxicity versus total body dose [cGy] graph with the data points of the twenty-one sample patients of Figure 12; and

Figure 15 is a toxicity versus total body dose-lean [cGy] graph of the data points of the twenty-one sample patients of Figure 12.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

5 According to the theory underlying the general method of the present invention, the body represents two major compartments, a "fat" compartment and a "lean" compartment and that the "lean" person resides within an outer shell of "fat". These related theories represent a major departure from other approaches to dosimetry. Accordingly, a calculation of the quantity of the patient which is "lean body mass" can be made. From this new mass and new shape, a new and more accurate radiation dose can be determined to the "lean body" using methods of least squares fitting of kinetic radioantibody or radiopharmaceutical clearance data and assumptions of non-uniform distribution of radioactivity between the two body compartments. From this is produced one simple assumption that all radioactivity resides in the "lean" compartment, while none resides in the fat compartment, which encases the "lean" compartment. With the further assumption that the bone marrow is part of the freely accessible "lean" compartment, a beta particle and photon dose to the lean compartment can be determined. It is further assumed in this approach that irradiation of the "fat" layers has either no significant or has little significant adverse effects on bone marrow function.

I. GENERAL METHOD

Figure 1 illustrates the relationship of the fat component of the individual with respect to the lean component. An individual can be thought of as two ellipsoids, with the length $x-1$ or $x-2$ and with $y-1$ or $y-2$. The outer ellipsoid, labelled OE, with the larger x and y dimensions represents fat plus lean mass, with a volume (in liters) approximately equal to the patient's weight (in kilograms). The inner ellipsoid, labelled IE, with the same aspect ratios, is defined in liters by the formulae:

$$45.5 + 0.91(\text{height}-152) = \text{Lean Body Mass (for women)}$$

$$48.0 + 1.06(\text{height}-152) = \text{Lean Body Mass (for men)}$$

(where height is in centimeters)

5 It should be understood that total Lean Body Mass could also be directly measured by CT, x-ray absorptiometry, immersion weighing, and other known methods. The total body absorbed dose is then determined for the lean body ellipsoid based on conventional calculations. It should also be understood that corrections for Compton scatter of photons from the fat compartment or some trace accumulation in the fat compartment are also possible, but need
10 not be included in the simplest application of the present method.

The steps of the method for applying the present invention are as follows, and reference may be had throughout the following explanation to Example 1 which appears below.

15 A "Proposed Lean Body Radiation Dose" is determined. This is a variable and can be selected from a wide range of possibilities. The proposed lean body dose shown in the "Data Entry" of Example 1 is 75 and is based on the particular antibody used. The value 75, however, should be interpreted as being a representative range. (It is to be understood that while Example 1 is directed to the use of an antibody, the methods of the present invention may
20 be more generally used with any protein or compound having specificity for a target cell or a target substance, provided the protein or compound is capable of carrying a radioactive marker or label. For example, newly developed phospholipidethers having cancer-cell specificity may be radiolabelled and used in the method of the present invention.)

25 Thereafter, the "Patient Lean Body Mass" is determined from the formula set forth above or other methods. In Example 1, the subject was a male, and the value (in kilograms) was found to be 65.00.

30 The "Tracer Dose" (in mCi) represents a the amount of radioactivity (the "Tracer Dose") that is initially administered to the patient. The course and timing of the elimination of the "Tracer Dose" is thereafter followed. The course of elimination is illustrated in Example 1 under the "Whole Body Probe Data".

As shown, the "Tracer Dose" was injected over a period of 40 minutes ("Start of Infusion: 3:50 PM; End of Infusion: 4:20 PM"). ~~A whole body radioactivity probe~~ is used to thereafter determine the amount of radioactive material still remaining in the body after certain intervals of time. (The whole body probe is only one of several possible ways of measuring the radioactivity in the patient. Other possible methods include a gamma camera, a geiger counter, whole-body counter, etc.)

In Example 1, the test intervals are separated by approximately 24 hours, as may be seen by reference to "Data Points" 1 through 8. Specifically, counts are done using the same radiation detection device from both anterior and posterior views. This is the so-called "conjugate view approach" and allows both front and back views of the patient and determination of a geometric mean of counts. ("P Intv" refers to length of the counting in seconds; the "Bkg counts" refers to background counts.)

Thereafter, and with reference to the "Data Analysis" of Example 1, a plot illustrating the disappearance of the radiation from the patient as determined by the probe is graphed. The plot of Example 1 is represented in Figure 2 showing time intervals (in hours) along the X-axis and the amount remaining along the Y-axis. On the "Data Analysis", ~~a calculation has been done~~ demonstrating the percentage of radioactive material (in this instance, radioactive iodine) that remains in the patient at a given time. With 100% of the dose being present at the beginning of the study, this amount is seen as disappearing over a period of time.

By referring to a trapezoidal integration determination (on the "Dosimetry Analysis" of Example 1), the area under the curve of the elimination graph (shown as an example in Figure 2) can be determined. ~~(This can also be done using the "Curve Fitting" approach also illustrated under "Dosimetry Analysis" which utilizes a series of curve fitting coefficients.)~~ This represents ~~accumulated~~ radiation exposure to the patient. With this amount known, the "Long Term Behavior Extrapolation" ("Data Analysis") is used to provide information as to how quickly the radioactive material is leaving the body.

(There are listed three "Options" listed: "last 2pts., last 3 pts., last 4 pts." This is from the tail end of the disappearance of a curve such as that shown in Figure 2. At "last 3 pts.", the extrapolated $T_{1/2}$ is 67.85 hours.)

Knowing the area under the curve and knowing, according to the provided example, that the lean body mass is 65 kilograms, a "Determination of Photo Absorbed Dose From Lookup Table" is then made. ("Lookup Table" follows "Dosimetry Analysis".) This determines what component of the dose is due to an absorbed photon in addition to the dose due to beta decay (electrons). The "Lookup Table" is photon energy specific. An example of I-131 is shown.

Now, knowing the size of the mass (in this instance, 65 kilograms) and the dimensions of the ellipsoid, the amount of radiation dose to lean body mass can be calculated. In Example 1, 60% of the radiation dose to lean body mass is due to electrons and 40% is due to photons. Accordingly, to produce the exemplary 75 rads, it is necessary in this particular case to give the patient a dose of 76.6 mCi, as the radiation dose to lean body mass/mCi is 0.9785. It is coincidental that the mCi dose approximates the rad dose.

As may be seen, the object of the present invention and the described steps is to identify the estimated dose in mCi (presented under "Estimated Dose" under "Dosimetry Analysis"). Overall, the "Estimated Dose" is determined by sequential sampling (in Example 1 particular case there were eight time points) using a radioactivity detector. The necessary probe data is determined by using either a trapezoidal integration formula or a curve fitting formula. This is directed to the determination of the area under the curve which is accumulated radiation. Then, using the body size, the amount of photons absorbed versus the amount of photons not absorbed becomes known as well as the beta component.

The general method of the present invention may be more fully understood by reference to the following example.

EXAMPLE 1

Data Entry

Patient: John Doe
 Reg. num.: 12345678
 Proposed Lean TB dose [cGy]: 75
 Patient height [cm]: 179
 Patient weight [kg]: 80.00
 Patient sex [M/F]: M
 Patient lean body Mass[kg]: 76.50
 Tracer Dose[mCi]: 5.100
 Therapy Dose[mCi]: 76.5
 Number of time points: 8

Study: Dx-1(686+16mg)
 Analysis Date: 22-Jun-06
 Start of Infusion: 14-Jun-06 3:50 PM
 End of Infusion: 14-Jun-06 4:20 PM
 Interval of Infusion: 0.50 hrs

Whole Body Counting Data:

Whole body probe data

Data Point	Date / time	Antl. counts	Post. counts	P Intvl[sec]	Bkg counts	Bkg Intvl[sec]	Pat Net(cps)
n-e-Inf bkg	24-Jan-00 12:00 PM	0	0	60.00	0	60.00	0.00
1	14-Jun-06 4:31 PM	47411	47391	60.00	80	60.00	0.00
2	15-Jun-06 8:12 AM	46881	38609	60.00	101	60.00	788.98
3	16-Jun-06 8:08 AM	38542	31381	60.00	101	60.00	707.39
4	17-Jun-06 8:15 AM	32076	25880	60.00	88	60.00	577.94
5	18-Jun-06 8:15 AM	23551	19913	60.00	83	60.00	478.73
6	19-Jun-06 8:50 AM	18945	16412	60.00	90	60.00	359.55
7	20-Jun-06 8:20 AM	16105	12582	60.00	91	60.00	292.38
8	21-Jun-06 8:10 AM	11838	9491	60.00	91	60.00	235.73
last time point value must go here							175.15
cpe at end of infusion =							788.68

Data Analysis

Patient: John Doe
 Reg. num.: 12345678
 Study: Dose 1 (685+15mg)
 Analysis Date: 22-Jun-96

Whole body probe data

Data Point	Time(hrs)	%I131	%ID	%ID/g	Trapezoidal cell integrals:
Start of Intra.	0.00	0.00	0.00	0.000000	
End of Intra.	0.50	99.82	100.00	0.001307	24.96
End of Intra.	0.50	0.00	0.00	0.000000	0.00
End of Intra.	0.50	0.00	0.00	0.000000	0.00
1	0.68	99.76	100.00	0.001307	9.14
2	16.37	89.53	94.94	0.001241	1494.33
3	40.30	73.15	84.51	0.001105	1946.74
4	64.42	60.59	76.32	0.000998	1612.68
5	89.42	45.51	62.69	0.000820	1328.23
6	114.00	37.01	55.68	0.000728	1014.22
7	137.50	28.84	48.83	0.000638	785.39
8	161.33	22.17	39.52	0.000517	619.71

Long Time Behavior Extrapolation: I-131 Tp 1/2 183.44 hrs

Time [hrs]	%I131	slope	Intercept	option	T 1/2 extrap	T 1/2 bld
0.00	0.00					
0.50	99.82					
0.50	0.00	-0.0125	5.1098	last 2 pts.	55.60	78.02
0.50	0.00	-0.0108	4.8588	last 3 pts.	63.99	95.61
0.68	99.76	-0.0099	4.7256	last 4 pts.	69.90	109.46
16.37	89.53					
40.30	73.15					
64.42	60.59					
89.42	45.51					
114.00	37.01					
137.50	28.84					
161.33	22.17					

Yields an extrap. T1/2: 63.99 [hrs]

Last time point value: 22.17 [%I131]

Dosimetry Analysis

Patient: John Doe Study: Dx-1(885+15mg) 22-Jun-98
 Reg. num.: 12345678 Analysis Date:

Whole body probe data

Trapezoidal Integration of %I-131:			
Integral to last data point:	8823.40	[%I131-hr]	
Int from last pt to Int(Textrap 1/2):	2046.81	[%I131-hr]	
Int %I-131(t)	10870.21	[%I131-hr]	
0			

Curve fitting of %ID: (biexponential)		
y = biexpfit(a,b,c,d)	Value	Error
a		
b		
c		
d		
ChiSq		
R		

Determination of photon absorbed dose from table lookup:

Pat't wt LBMt	76.50 [kg]
$\Sigma \Delta e(\text{pho})$:	77.00 [rounded to nearest kg]
$\Sigma \Delta e(\text{elec})$:	0.281010 [g-rad] $\mu\text{Ci-hr}$
	0.408500 [g-rad] $\mu\text{Ci-hr}$
$\Sigma \Delta e(\text{total})$:	0.689510 [g-rad] $\mu\text{Ci-hr}$

Curve Trapezoidal fitting Integration			%difference
Residence Time:	0.00	108.70 [hrs]	#DIV/0!
Effective T1/2:	0.00	76.35 [hrs]	
Kinetics:	AUC(0,-):	#DIV/0!	[%ID-hr]
	AUMC(0,-):	#DIV/0!	[%ID-hr ²]
Mean system res time:	#DIV/0!	[hrs]	

Dosimetry Results:

Estimated Dose:	Electron		Photon		Total
	frac of total		frac of total		
	0.5805	59%	0.3983	41%	0.9788 [rad/mCi]
	0.01569		0.01079		0.02648 [cGy/MBq]
76.5 mCi therapy:	44.4		30.6		75.0 [rad]
2832.3443 MBq					75.0 [cGy]

TABLE (LOOKUP)

Mass (kg)	$\Sigma \Delta e$ (photon)
1	0.079500
2	0.093200
3	0.106800
4	0.120600
5	0.129250
6	0.137800
7	0.144700
8	0.151500
9	0.156750
10	0.162000
11	0.166480
12	0.170960
13	0.174980
14	0.178010
15	0.182620
16	0.186230
17	0.189480
18	0.192730
19	0.195660
20	0.198800
21	0.201270
22	0.203840
23	0.206380
24	0.208830
25	0.211080
26	0.213320
27	0.215410
28	0.217480
29	0.219450
30	0.221400
31	0.223250
32	0.225110
33	0.226870
34	0.228640
35	0.230330

Cubic spline interp
lookup table:

$\Sigma \Delta e$ for photons from 1-131
activity uniformly distributed
in ellipsoid:

Mass (kg)	$\Sigma \Delta e$ (photon)	$\Sigma \Delta e$ (elctm)
2	0.0932	0.4085
4	0.1206	
6	0.1379	
8	0.1515	
10	0.1620	
20	0.1986	
30	0.2214	
40	0.2394	
50	0.2528	
60	0.2645	
70	0.2748	
80	0.2838	
90	0.2922	
100	0.2994	
120	0.3136	
140	0.3264	
160	0.3388	
180	0.3495	
200	0.3604	

75	0.278280	114	0.309400	153	0.334450
76	0.280150	115	0.310110	154	0.335050
77	0.281010	116	0.310820	155	0.335650
78	0.281870	117	0.311520	156	0.336250
79	0.282730	118	0.312220	157	0.336850
80	0.283600	119	0.312910	158	0.337440
81	0.284480	120	0.313600	159	0.338020
82	0.285360	121	0.314280	160	0.338600
83	0.286240	122	0.314950	161	0.339170
84	0.287120	123	0.315620	162	0.339740
85	0.288000	124	0.316280	163	0.340300
86	0.288870	125	0.316930	164	0.340870
87	0.289720	126	0.317590	165	0.341420
88	0.290570	127	0.318230	166	0.341970
89	0.291390	128	0.318880	167	0.342520
90	0.292200	129	0.319510	168	0.343070
91	0.292970	130	0.320150	169	0.343610
92	0.293740	131	0.320780	170	0.344150
93	0.294470	132	0.321410	171	0.344690
94	0.295210	133	0.322040	172	0.345230
95	0.295910	134	0.322660	173	0.345760
96	0.296620	135	0.323280	174	0.346300
97	0.297320	136	0.323910	175	0.346830
98	0.298010	137	0.324530	176	0.347360
99	0.298710	138	0.325160	177	0.347900
100	0.299400	139	0.325780	178	0.348430
101	0.300100	140	0.326400	179	0.348970
102	0.300800	141	0.327020	180	0.349500
103	0.301510	142	0.327650	181	0.350040
104	0.302220	143	0.328270	182	0.350570
105	0.302840	144	0.328890	183	0.351110
106	0.303660	145	0.329520	184	0.351650
107	0.304380	146	0.330140	185	0.352200
108	0.305100	147	0.330760	186	0.352740
109	0.305820	148	0.331380	187	0.353280
110	0.306540	149	0.332000	188	0.353830
111	0.307260	150	0.332620	189	0.354370
112	0.307970	151	0.333230	190	0.354920
113	0.308690	152	0.333840	191	0.355460

182	0.356010
183	0.356580
184	0.357110
185	0.357650
186	0.358200
187	0.358750
188	0.359300
189	0.359850
200	0.360400

II. MODIFIED METHOD

The method for determining the number of millicuries to be administered to a patient so as to deliver a given centigray (cGy) dose to either the patient's lean body or the patient's total body set forth above may be modified. The following steps are involved according to the modified method of the present invention:

- (1) Injecting a radioactive tracer into a patient;
- (2) determining radiation levels in the whole body;
- (3) calculating a geometric mean;
- (4) determining the percent-injected activity remaining in the body at each time point;
- (5) plotting the percent-injected activity versus calculated time from infusion on a log-linear graph;
- (6) determining the effective half-life (and the rate of clearance) from the log-linear graph by identifying the intersection of the best fit line with the 50% injected activity line;
- (7) cross-indexing the effective half-life value with the patient's body weight (either total body mass for total body dose or lean body mass for total body dose-lean) on either a graph or on a numerical chart to identify the actual amount of therapeutic millicuries per centigray [cGy] (delivered to total body mass or lean body mass); and
- (8) multiplying the determined amount of therapeutic millicuries per centigray [cGy] (delivered to total body mass or lean body mass) by the amount of desired centigray (to total body mass or lean body mass) to be administered.

These steps along with their associated substeps are set forth in detail as follows and are to be read in correlation with the several figures discussed in conjunction therewith.

DETERMINATION OF RATE OF CLEARANCE

Determining the rate of clearance of an injected dose of a particular radiopharmaceutical is critical to the determination of the amount of therapeutic dose to be administered. A person who clears the injected dose quickly would receive a relatively large therapeutic dose of the particular radiopharmaceutical drug as compared to a person who clears the injected dose less quickly. This is simply because of residence time - the longer the radiopharmaceutical is proximate to the disease site, the less need be administered. Quick clearance translates into brief exposure to the radioactive element and less effective treatment of the disease. (Other factors determine the administered radioactivity dose, including the size of the patient and the desired total centigray amount.)

Rate of clearance according to the modified method of the present invention is determined by administering an amount of a "tracer dose" to the patient. The tracer dose represents a small amount of radioactivity attached to an antibody. As noted above, the methods of the present invention are not limited to use of an antibody. Rather, any protein or compound having specificity for a target cell or a target substance, provided the protein or compound is capable of carrying a radioactive marker or label, may be used according to the various methods disclosed herein.

The particular protein (such as an antibody) or compound (such as a phospholipidether) is selected according to its specificity to a target substance (such as an antigen) or to a target cell (such as a cancer cell). In light of the known utility of antibodies and by way of example, the following discussion will be based on the use of an antibody.

The "tracer dose" (in mCi) represents the amount of radioactivity that is initially administered to the patient. (The "tracer" aspect of this dose does not refer to a trace amount of antibody, but rather to the trace amount of radioactive material attached to the antibody. The antibody mass is delivered during the stage of estimating the rate of clearance in the same amount as in therapy, however, the amount of radioactivity administered is lower to prevent

toxicity to the system. Experimentation has shown that the tracer dose is; in fact, a reliable predictor of the therapeutic dose. Special measurements taken after therapy initially based upon a tracer dose has shown that the kinetics of clearance of the antibody with the tracer amount generally predict the kinetics of clearance of the therapeutic amount; in fact, these results are substantially identical.)

After administration of the tracer dose, the course of timing of the elimination of the tracer dose is thereafter followed. The tracer dose is first injected into the patient over a period of time, such as 40 minutes. Thereafter a probe is used to determine anterior and/or posterior counts, thus quantitatively demonstrating the amount of radioactivity remaining in the body after certain intervals of time. Measurements may be taken by any of several devices including a sodium-iodine probe, a gamma camera, a geiger counter, a whole-body counter, etc. Measurements are taken once approximately every 24 hours over a course of several days. Infusion stop and start times are recorded, as are counts taken for elimination over several 24-hour periods. The relevant intermediate numerical values are entered onto a worksheet such as that illustrated in Figure 3.

As an alternative to recording time points for each day of several days, as few as three (and possibly two) time points may be used to determine the shape and slope of the clearance curve of radioactivity from the body. This was verified through experimentation on twenty-eight patients who each received 700 mg total of anti-B-1 by comparing the dose calculated from eight time data points according to the computation methodology set forth above in the general method against the graphic-tabular approach and three time points of the modified method of the present invention. The comparative results are set forth in Figure 4. The correlation produced an r-value of 0.983 with a mean % difference in calculated mCi dose between the two methods being 3.33%. As illustrated in the accompanying Figure 4, the slope is 0.99 and the intercept is essentially 0. Accordingly, using the present graphic-

tabular method, three probe determinations taken at 0, 3, and 7 days may be used to calculate patient dose.

Once the counts are recorded over the requisite time period, the geometric mean is obtained. This may be done by taking readings from daily NaI probe measurements, but also may be done by relying upon readings from anterior and posterior conjugate view gamma camera imaging. When the latter approach is used, a geometric mean is obtained for each set of recorded anterior and posterior counts (representing an individual time point) is determined by the following formula:

$$\text{geometric mean} = \sqrt{\text{anterior count} \times \text{posterior count}}$$

The determined geometric mean is not corrected for radioactive decay. Once the geometric mean is known, net geometric mean counts are calculated by subtracting background counts according to the following formula:

$$\text{geometric mean (net)} = \text{geometric mean} - \text{bkg}$$

For example, if the background count is 100 cpm and the patient's count is 2000 cpm, then the net counts to the patient would be 1900 cpm.

Thereafter, the percent-injected activity remaining in the body at each time point is determined by forming a ratio to the geometric mean at the initial time point (again, not corrected for radioactive decay) according to the following:

$$\text{percent-injected activity (at each time point)} = \frac{\text{geometric mean (net)}}{\text{geometric mean (initial)}} \times 100\%$$

Once the percent-injected activity for each time point is known, these values are entered into a graph to determine total body effective half life. Figure 5 is a blank graph consisting of a log linear graph onto which the pertinent values are to be marked. The percent-activity is read along the Y-

axis (log scale) and the time from injection (in hours) is read along the X-axis (linear scale).

Figure 6 is the graph of Figure 5 now completed and showing the relevant values of two patients. Patient "A" is denoted by a series of eight open boxes representing measurements of percent-injected activity recorded over a period of 160 hours. Patient "B" is denoted by a series of eight closed circles also representing measurements of percent injected activity recorded over the same period of time. Lines are drawn through the respective series of open boxes or closed circles to establish the respective curves.

The effective half-life for each patient is determined by identifying the point at which the respective curves intersect the 50% injected activity level, indicated by a horizontal line on the charts of both Figures 5 and 6. This point represents the effective half-life, or $T_{1/2}$ -effective. Given, for example, Patient A, $T_{1/2}$ -effective is 88 hours, while $T_{1/2}$ -effective for Patient B is 47 hours. Obviously, Patient A clears the injected dose more slowly than does Patient B.

TOTAL BODY DOSE VERSUS TOTAL BODY DOSE-LEAN

~~The present invention improves on the known techniques~~ of determining the optimal dose for administration of therapeutic radiopharmaceuticals in several ways. One such improvement rests in the unsettling of the previously-held notion that doses of therapeutic radiation could be determined based on patient weight. This notion fails to take into account several variables, including "fat" versus "lean" compartments and the related effects of "total body dose" versus "total body dose-lean".

The body represents two major compartments, a "fat" compartment and a "lean" compartment. The corollary to this is that the "lean" person resides within an outer shell of "fat". These related theories represent a major departure from other approaches to dosimetry. Accordingly, a calculation of the quantity of the patient which is "lean body mass" can be made. From this new mass and new shape which essentially isolates the "lean" from the "fat", a new and more accurate radiation dose can be determined to the "lean body"

using methods of least squares or graphical fitting of kinetic radioantibody clearance data and assumptions of non-uniform distribution of radioactivity between the two body compartments.

Figure 7 demonstrates the significance of distinguishing between "lean" and "fat" body compartments. Figure 7 is a "fused" image of a cross-section of a patient following administration of radiolabelled antibodies. The image is produced by a fusion computer program that superimposes a CT image slice corresponding to a SPECT image slice. Details of this procedure and its application are set forth in an article by K.F. Koral et al. and entitled CT-SPECT FUSION PLUS CONJUGATE VIEWS FOR DETERMINING DOSIMETRY IN IODINE-131-MONOCLONAL ANTIBODY THERAPY OF LYMPHOMA PATIENTS (J. Nucl. Med., Vol. 35, No. 10, October 1994, pps. 1714-1720). Generally, Figure 7 illustrates a central body compartment that includes the major organs such as the kidneys and spleen. The individual images are scaled by a computer so they substantially overlap when superimposed. The lighter areas are areas of relatively high amounts of radioactivity, while the darker areas are areas of low radioactivity.

With respect to Figure 7, a tumor, T, is shown in close association with the right kidney, labelled Rt K. Other organs illustrated include the aorta, A, the left kidney, Lf K, and the spleen, Sp. The patient's external body outline, labelled O, is illustrated, having thereupon a marker, M, to demonstrate the position of the body outline O. The outline O is the outer boundary of the patient and therefor represents the air-skin interface. The black area is mainly non-lean tissue, with the gray areas being the central area or the leaner body mass. As illustrated, there is a considerable amount of radioactivity in the vascular or lean component where antibody presence is the greatest. There is comparatively little radioactivity in the non-lean tissue, as illustrated by the black color. The patient illustrated in Figure 7 is a relatively large person having an excess amount of body fat. The body outline O would be closer to the internal organs on a thinner person.

While clearly illustrating the differences in uptake of the radiolabelled antibody between the lean and non-lean compartments, Figure 7 also demonstrates how it is generally not possible to target the disease site itself. While careful selection of a particular antibody will minimize cross-reaction with normal tissue, interaction (specific or non-specific) with non-disease tissue invariably results, in that as antibodies are directed to the tumor through blood vessels, the same vessels will naturally transport the antibodies in places other than to the disease site. Figure 7 also illustrates the simple assumption of the present invention that all (or substantially all) radioactivity resides in the "lean" compartment, while none (or virtually none) resides in the "fat" compartment, which encases the "lean" compartment. With the further assumption that the bone marrow is part of the freely accessible "lean" compartment, a beta particle dose and photon dose to the "lean" compartment can be determined. These estimations are important, in that the total amount of energy deposited in an individual as a result of radioactive decay is the "radiation dose" which is adjusted per unit weight for the particular individual or tissue and for a particular radioactive material. A specific example is the radioactive material I-131 which is both a beta emitter and a gamma emitter.

Following injection of an antibody labelled with I-131, for example, the central "lean" compartment of the body emits both beta and gamma particles. The beta particles are more or less confined within the compartment, while only some of the gamma particles are so confined. The extent to which the gamma particles are confined depends on the sizes of the "lean" and "fat" compartments. Some of the gamma particles strike some fat tissue and are scattered, returning to the "lean" compartment. Accordingly, not only does accurate quantification of the "lean" and "fat" compartments assist in eliminating reliance on the pure weight of a body in determining dose administration, an understanding of these compartments with respect to the individual patient also aids in determining, with greater accuracy, the "tracer dose" and its elimination.

Accordingly, it may now be understood that total body dose (TBD) assumes that all radioactivity is uniformly distributed throughout the patient's total body mass, and that all beta/electron energy is absorbed in the total body mass. TBD calculations for photon energy deposition are made from absorbed fractions of emissions of the radioactive material (for example, I-131) in the ellipsoid of mass equal to the total body mass. Conversely, total body dose - lean (TBD-Lean) is modeled as a lean-body mass ellipsoid surrounded by a fat-layer ellipsoid shell. TBD-Lean assumes that all radioactivity is uniformly distributed throughout the patient's lean body mass, since there is little tracer distribution to fat. In the TBD-Lean model, all beta/electron energy is absorbed in the lean-body mass, and photon energy is absorbed in lean-body mass ellipsoid volume. This said, it is clear that the more obese the patient, the more important dosage be based on the TBD-Lean model. Conversely, dosage for a relatively thin person could be reliably based on the TBD approach. However, regardless of the approach, the present method of determining optimal radiation dose could be used with either the TBD or the TBD-Lean model, with the latter model providing the better determination, particularly in the case of the obese patient.

Figure 8 illustrates the relationship of the fat component of the individual with respect to the lean component and accordingly is a visually simplified version of the actual section shown in Figure 7. An individual can be thought of as two ellipsoids, with the length x-1 or x-2 and with y-1 or y-2. The outer ellipsoid, labelled OE, with the larger x and y dimensions represents fat plus lean mass, with a volume (in liters) approximately equal to the patient's weight (in kilograms). The inner ellipsoid, labelled IE, with the same aspect ratios, is defined in liters by the following formulae that determine "lean body mass" (LBM):

$$45.5 + 0.91 \times (\text{height [in cm]} - 152) = \text{LBM for females}$$

$$48.0 + 1.06 \times (\text{height [in cm]} - 152) = \text{LBM for males}$$

It should be understood that total LBM could also be directly measured by CT, x-ray absorptiometry, immersion weighing, and other known methods. The

total body absorbed dose is then determined for the lean body ellipsoid based on the following methods. It should also be understood that corrections for Compton scatter of photons from the fat compartment or some trace accumulation in the fat compartment are also possible, but need to be included in the simplest application of the present method. Following this general guideline, the method of determining the patient's LBM of the above-described general method is followed.

DETERMINATION OF THE WHOLE BODY DOSE

With the effective half life or $T_{1/2}$ -effective determined from tracer study, the whole body dose may be calculated. By "whole body dose", it is meant that these calculations are made for the whole body or for the lean body mass component of the whole body.

The calculations of the whole body dose according to the modified method are based on the assumption that the radioantibody is uniformly distributed throughout the patient (or the lean body mass compartment) following tracer injection and that the tissues are of uniform water density. Accordingly, determining the patient's mass (or lean body mass as set forth above) determines the assumed water content and patient volume for dosimetric calculations.

The "total body residence time" is an integral of the time activity curve for the total body divided by the injected activity according to the following formula:

The relative contributions of electron and photon radiation are summed to produce the total body radiation dose ([cGy]/mCi) administered. The formula for this determination is as follows, where the total body dose is the sum of

electron energy plus photon energy deposited in an ellipsoid having a mass m_{TB} :

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This equation can be solved for A_T , the therapy activity in mCi to impart a given total body dose, D_{TB} .

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These individual equations could be solved manually. However, it is preferred that the equations be reduced to graphical and tabular (numerical chart) formats, as illustrated in Figures 9a - 9p (for use in the graphical method) and Figures 10a - 10h (for use in the tabular method). A three-dimensional representation of the graphical method is illustrated in Figure 11. Such reductions greatly reduce the need for calculation and allow the method

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To use the graphs of Figures 9a - 9p, the known effective half-life is cross-indexed with the patient's weight. The amount of therapeutic millicuries/cGy (for either total body dose or total body dose-lean) is set forth along the Y-axis, and the physician reads along the graph to the left to make this determination. To use the tables of Figures 10a - 10h, again the known effective half-life is cross-indexed with the patient's weight. The value at the intersection of the weight and $T_{1/2}$ -effective is the amount of therapeutic millicuries/cGy.

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Once the amount of therapeutic millicuries/cGy is established, this value is multiplied by the amount of desired centigray to be administered to treat a particular disease. These amounts are well known to those skilled in the art, but are not uncommonly in the 50-90 cGy range for whole-body dose.

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Both the general and modified methods of the present invention may be more fully understood by reference to the following example.

EXAMPLE 2

~~A phase-I dose-escalation trial~~ of I-131 labelled B1 antibody for the treatment of patients with non-Hodgkin's lymphoma was undertaken using a dose-escalation scheme designed around increasing levels of total body radiation dose. The overall results of the studies of 21 patients are set forth in the table of Figure 12. (The study began with 34 patients, hence the listing in the left-hand column of patient numbers with some patient numbers missing. Some of the missing patients, i.e., nos. 3, 11, 12, 17, 18, 20-23, 25, 26, 30, and 33, were bone marrow transplant patients or were patients who were subsequently not treated for various reasons, e.g., development of human antimouse antibody.)

Hematological toxicity was the major toxicity observed in the 21 patients studied that received radioimmunotherapy. Patients were treated with radioimmunotherapy doses calculated from tracer dosimetry studies (Nal probe) to deliver doses to the whole body ranging from 25 to 85 cGy. Hematological toxicity after treatment was assessed by the NCI common criteria, grades 0-4. Nine patients had no toxicity, 5-grade-1, 3-grade-2, 2-grade-3, and 2-grade-4 (grade 4 is the most severe). Total body dose was estimated by modeling the patient as a uniform activity distribution in an ellipsoid for the purpose of calculating the energy absorbed fraction of photons from I-131 decay. The parameter of the present invention, the Total Body Dose-Lean was introduced to account for the fact that obese patients can be modeled as an outer shell of fat (with little radioantibody accumulation) surrounding the active lean body mass. Irradiation of the fat layer would presumably have little effect on hematologic toxicity. Blood clearance and dose was determined from actual tracer blood samples. Marrow residence time was estimated using the assumption that specific activity in marrow is 30% of the specific activity in blood. Resulting correlation between estimated dose parameters from the tracer studies and hematological toxicity grade were as follows:

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<u>Dose Parameter</u>	<u>r-value</u>	<u>p-value (N=21)</u>
blood-dose	0.337	0.146
marrow-dose	0.421	0.064
mCi/kg	0.270	0.236
TBD	0.430	0.052
TBD-lean	0.523	0.015

The TBD-lean correlated best with resulting toxicity following radioimmunotherapy in this patient group, offering a clear improvement over estimates of blood, marrow or TB dose.

The improvement according to the present invention is clearly observable by reference to the graphs of Figures 13 through 15. With respect first to the graph of Figure 13, dosage based on simple mCi per Kg of patient weight is set forth. The toxicity level correlates poorly with mCi/Kg due to the assumption of uniform distribution in the patient's total body mass, and also clearance kinetics are not taken into account. Figure 14 discloses a graph similar to that of Figure 13, but based upon total body dose (TBD) [cGy]. As illustrated, the toxicity grade from the administered dose correlates better with TBD than for the less exact method that produced the graph of Figure 13. Finally, Figure 15 discloses a graph similar to those of Figures 13 and 14, but illustrating results produced from reliance on the total body dose-lean (TBD-Lean) [cGy] method. The grade of toxicity from the administered dose is best predicted by the TBD-Lean method than that for the method based on total body dose (shown in Figure 14) and also the method based simply on mCi/body weight (shown in Figure 13).

Those skilled in the art can now appreciate from the foregoing description that the broad teachings of the present invention can be implemented in a variety of forms. Therefore, while this invention has been described in connection with particular examples thereof, the true scope of the invention should not be so limited since other modifications will become apparent to the skilled practitioner upon a study of the drawings, specification and following claims.

WHAT IS CLAIMED IS:

1. A method of establishing the optimal effective radiation dose in mCi for treatment of disease in a patient, said method comprising the steps of:
establishing the rate of clearance of a tracer dose from the patient's
5 body;
identifying the effective half-life value of said tracer dose in the patient
based on said rate of clearance;
determining the actual amount of therapeutic mCi per cGy based on
the effective half-life of said tracer; and
10 multiplying said actual amount of therapeutic mCi per cGy by the
amount of desired cGy to be administered.

2. The method of establishing the optimal effective radiation dose of Claim 1, including the further step of determining said actual amount of therapeutic mCi by cross-indexing said effective half-life value with the patient's body weight.

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3. The method of establishing the optimal effective radiation dose of Claim 2, including the further step of cross-indexing said effective half-life value with the patient's total body mass for a total body dose.

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4. The method of establishing the optimal effective radiation dose of Claim 2, including the further step of cross-indexing said effective half-life value with the patient's lean body mass for a total body dose-lean.

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5. The method of establishing the optimal effective radiation dose of Claim 1, including the further steps of injecting a radioactive tracer into the patient and determining a radiation level for said injected radioactive tracer.

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6. The method of establishing the optimal effective radiation dose of Claim 5, including the further step of calculating a geometric mean based on said determined radiation level.

7. The method of establishing the optimal effective radiation dose of Claim 6, wherein said geometric mean is based upon NaI probe measurements.

5 8. The method of establishing the optimal effective radiation dose of Claim 6, wherein said geometric mean is based upon anterior or posterior conjugate view gamma camera imaging data.

10 9. The method of establishing the optimal effective radiation dose of Claim 1, including the further step of determining the percent-injected activity remaining in the patient's body across a plurality of time intervals.

15 10. The method of establishing the optimal effective radiation dose of Claim 9, including the further step of plotting said percent-injected activity versus calculated elimination time from infusion on a log-linear graph.

20 11. The method of establishing the optimal effective radiation dose of Claim 10, wherein said log-linear graph includes a 50% injected activity line, said method including the further step of determining said effective half-life from said log-linear graph by identifying the intersection of the best fit line with said 50% injected activity line.

12. The method of establishing the optimal effective radiation dose of Claim 1, including the further step of cross-indexing said effective half-life with the patient's body weight on a graph having a first axis and a second axis substantially perpendicular to said first axis, said first axis having increments of Rx mCi/cGy and said second axis having increments of body mass to identify the actual amount of therapeutic mCi.

13. The method of establishing the optimal effective radiation dose of Claim 1, including the further step of cross-indexing said effective half-life with the patient's body weight on a table having a first axis and a second axis substantially perpendicular to said first axis, said first axis having increments of body mass and said second axis having increments of effective half-life to identify the actual amount of therapeutic mCi.

14. A method of establishing the optimal effective radiation dose for treatment of disease in a patient, said method comprising the steps of:
establishing the rate of clearance of a tracer dose from the patient's body;
identifying a numerical value based on said rate of clearance;
determining the actual amount of therapeutic mCi per cGy based on said numerical value by cross-indexing said numerical value with the patient's body weight; and
multiplying said actual amount of therapeutic mCi per cGy by the desired amount of cGy to be administered.

15. The method of establishing the optimal effective radiation dose of Claim 14, including the further step of identifying the effective half-life value of said tracer dose in the patient based on said rate of clearance.

5 16. The method of establishing the optimal effective radiation dose of Claim 15, including the further step of determining said actual amount of therapeutic mCi by cross-indexing said effective half-life value with the patient's body weight.

10 17. The method of establishing the optimal effective radiation dose of Claim 16, including the further step of cross-indexing said effective half-life value with the patient's total body mass for a total body dose.

15 18. The method of establishing the optimal effective radiation dose of Claim 17, including the further step of cross-indexing said effective half-life value with the patient's lean body mass for a total body dose-lean.

19. A method of establishing the optimal effective radiation dose for treatment of disease in a patient, said method comprising the steps of:
identifying the effective half-life value of a tracer in the patient; and
determining the actual amount of therapeutic mCi based on the effective half-life of said tracer.

20. The method of establishing the optimal effective radiation dose of Claim 19, including the further step of multiplying said actual amount of therapeutic mCi per cGy by the amount of desired cGy to be administered.

21. The method of establishing the optimal effective radiation dose of Claim 1, wherein said step of determining the actual amount of therapeutic mCi per cGy is also based on the patient's total body mass.

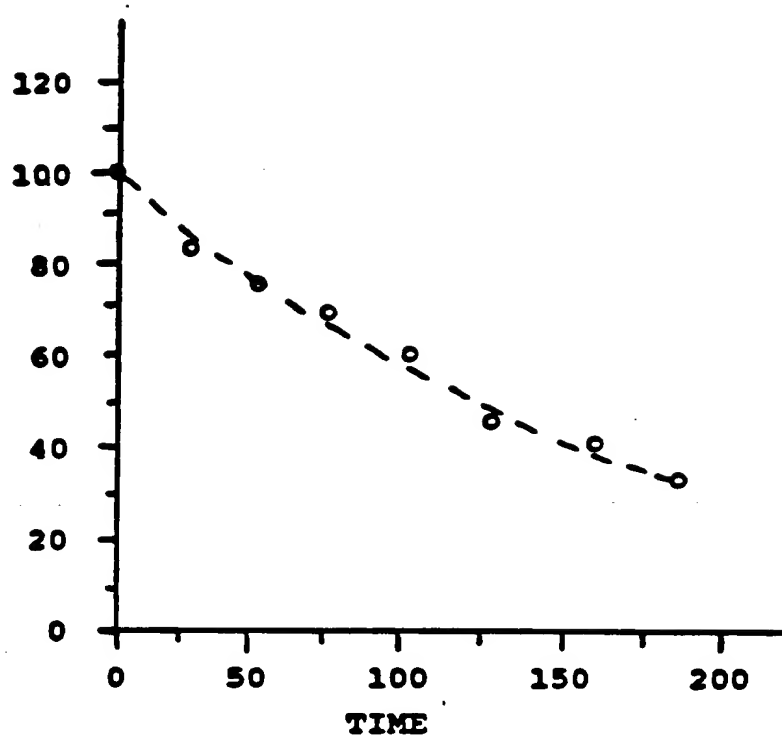
22. The method of establishing the optimal effective radiation dose of Claim 1, wherein said step of determining the actual amount of therapeutic mCi per cGy is also based on the patient's lean body mass.

23. A method of establishing the optimal effective radiation dose in mCi for treatment of disease in a patient, said method comprising the steps of:
establishing the rate of clearance of a tracer dose from the patient's body;
identifying the effective half-life value of said tracer dose in the patient based on said rate of clearance;
determining the actual amount of therapeutic mCi per cGy based on the effective half-life of said tracer;
multiplying said actual amount of therapeutic mCi per cGy by the amount of desired cGy to be administered; and
administering the radiation dose.

24. Use of an apparatus for establishing the optimal effective radiation dose in mCi for treatment of disease in a life form comprising means for establishing the rate of clearance of a tracer dose from the life form, means for identifying the effective half-life value of said tracer dose in the life form based on said rate of clearance, means for determining the actual amount of therapeutic mCi per cGy based on the effective half-life of said tracer, and means for multiplying said actual amount of therapeutic mCi per cGy by the amount of desired cGy to be administered.

25. An apparatus for establishing the optimal effective radiation dose in mCi for treatment of disease in a patient, said apparatus comprising:
means for establishing the rate of clearance of a tracer dose from the patient's body;
means for identifying the effective half-life value of said tracer dose in the patient based on said rate of clearance;
means for determining the actual amount of therapeutic mCi per cGy based on the effective half-life of said tracer; and
means for multiplying said actual amount of therapeutic mCi per cGy by the amount of desired cGy to be administered.

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**Fig. 2**

Integ. to last data point=
2882.67 [t]131-hr]

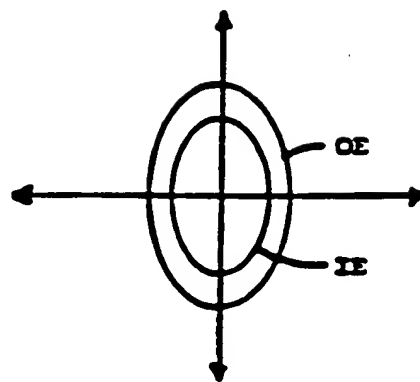
**Fig. 1**

Fig. 3**Diagnostic Total Body Clearance**

Patient: _____ Patient Lean Body (or Total Body) mass: _____ Kg
 Infusion Date/Time: _____ Projected TB-lean (or TB) dose: _____ cGy
 Injected activity: _____ mCi

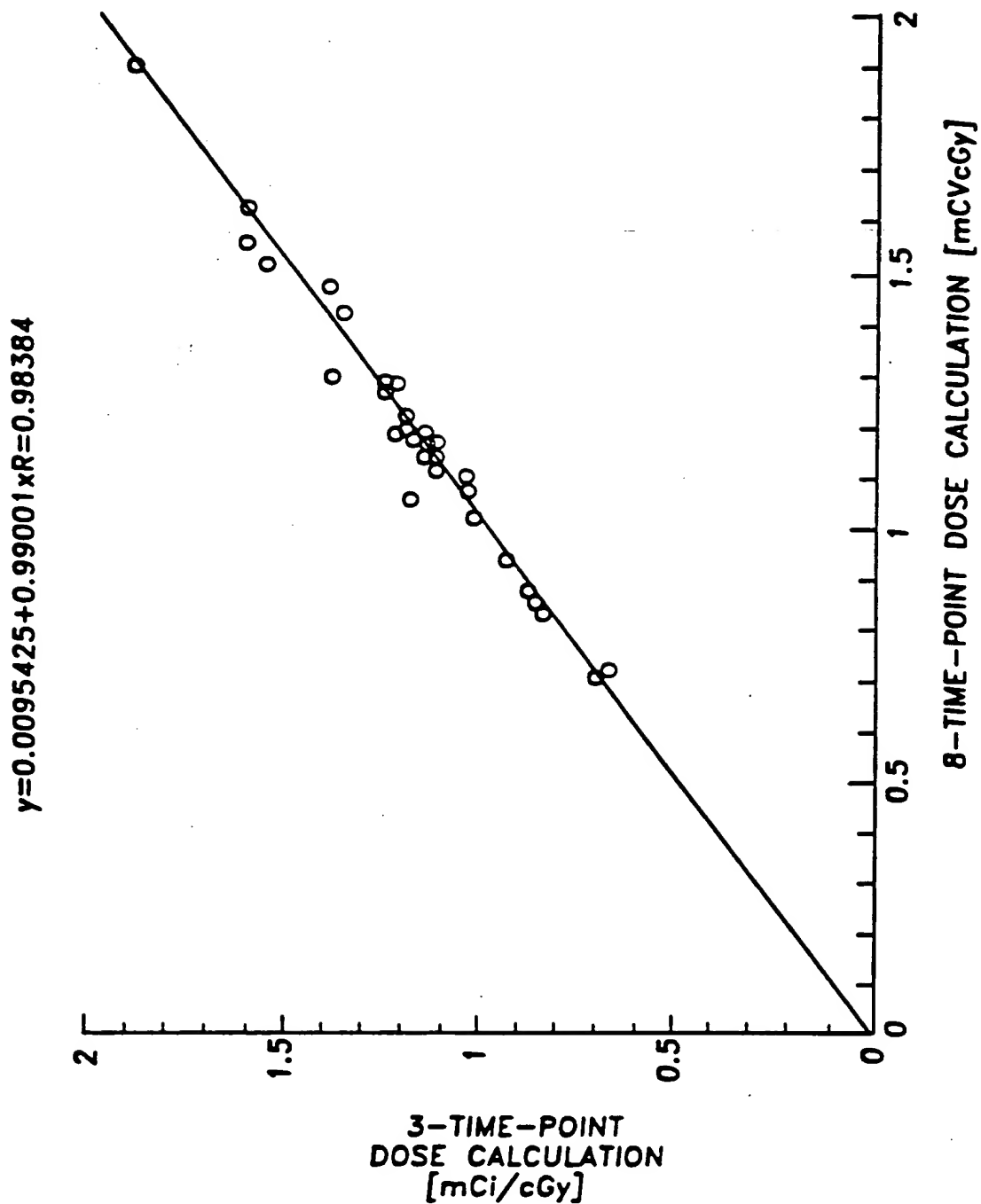
	time post infusion [hrs]	anterior whole body	posterior whole body	background	GM	GMnet	% injected activity
nominal time point							
immed post infusion							
1 day post							
2 day post							
3 day post							
4 day post							
5 day post							
6 day post							
7 day post							

Effective half life: _____ hrs
 A_0 (from table lookup): _____ mCi/cGy
 Prescribed therapy activity (for TBdose-lean or TBdose) = $A_0 \cdot$ Projected TB-lean dose: _____ mCi

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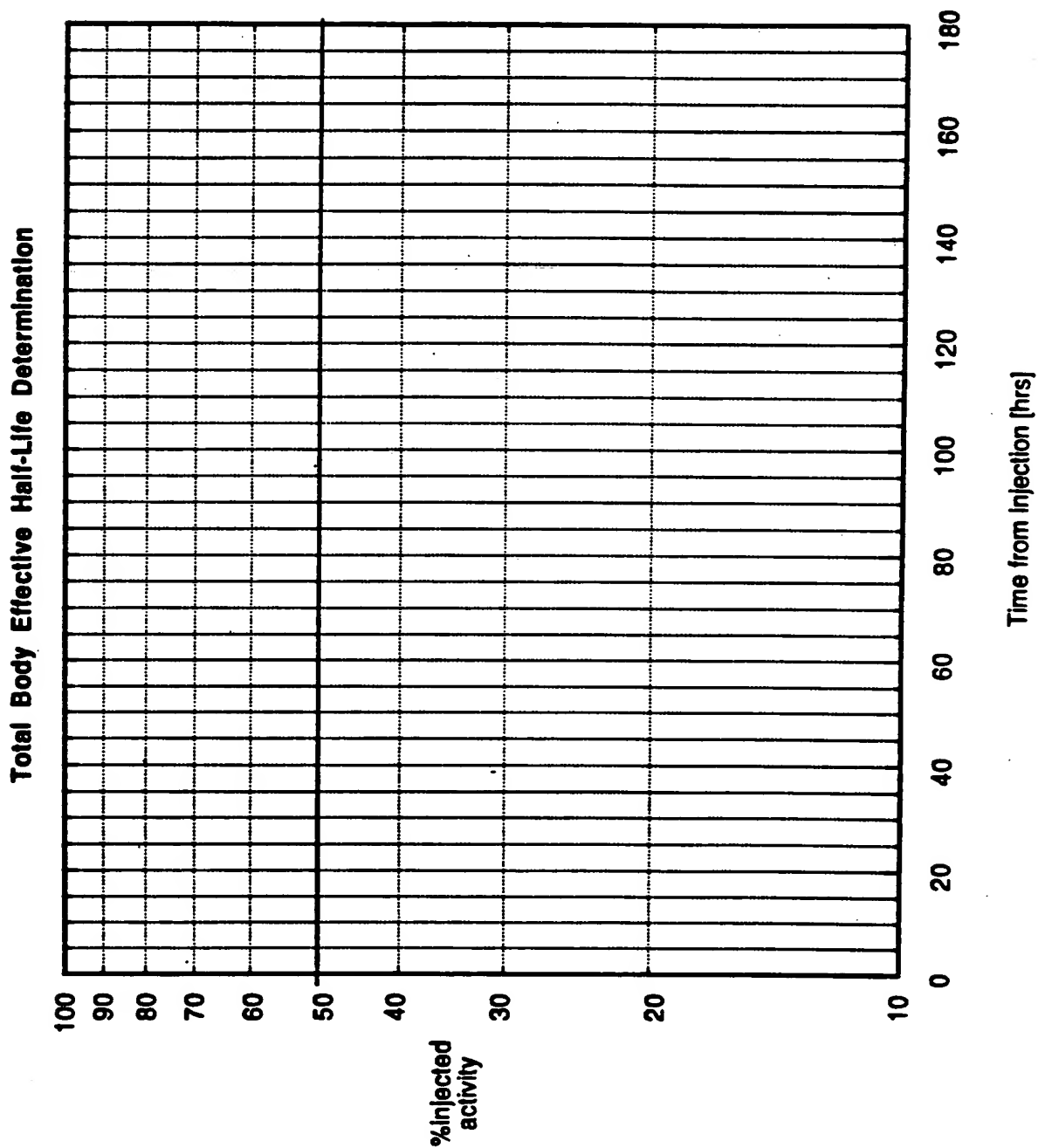
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Fig. 4



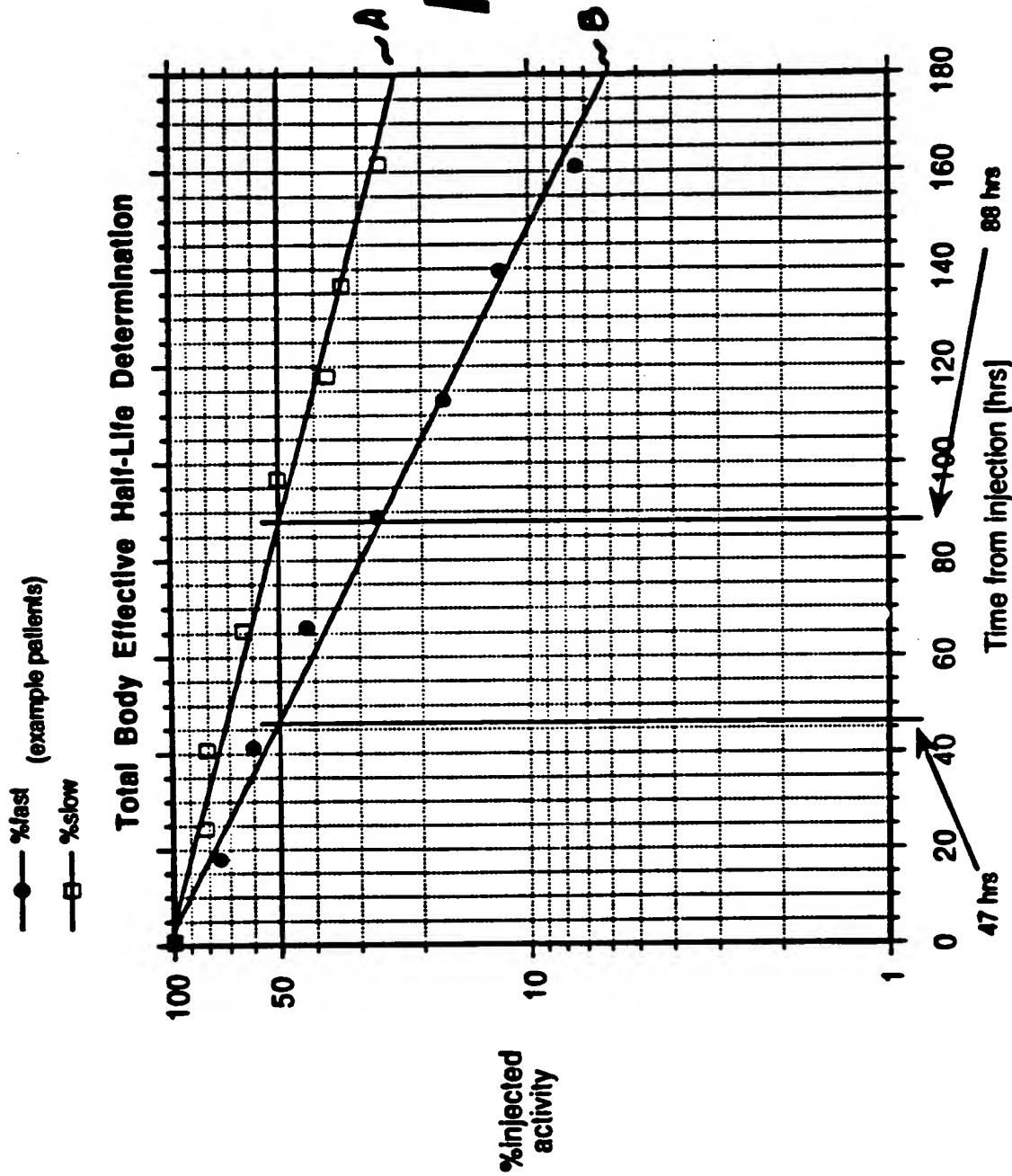
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Fig. 5



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Fig. 6



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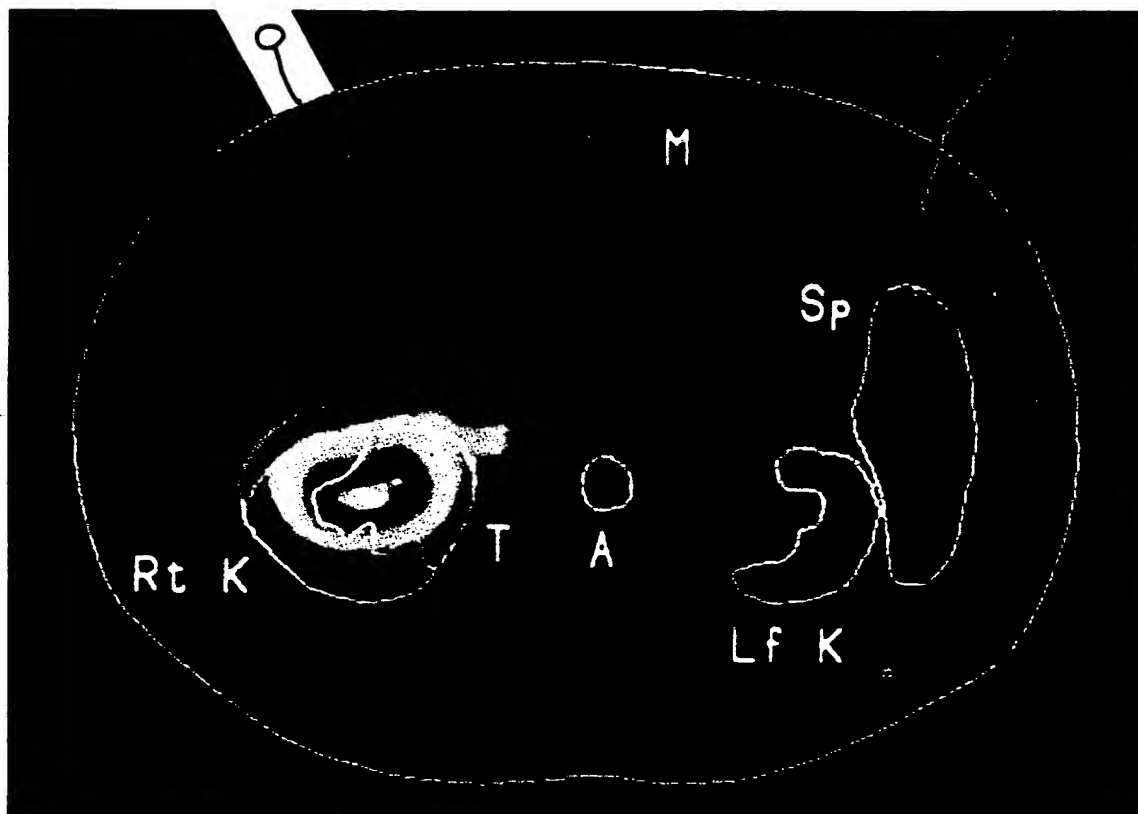


Fig. 7

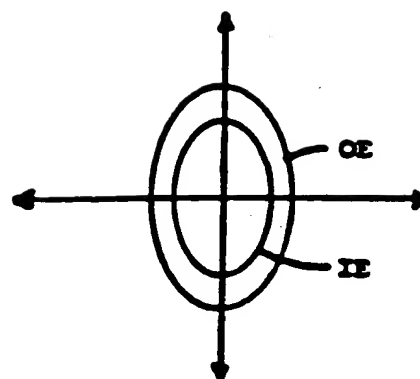


Fig. 8

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Rx Activity per cGy from 30hr < $T_{1/2}$ < 49hr and 40Kg < $M_{TB \text{ or } LB}$ < 60Kg

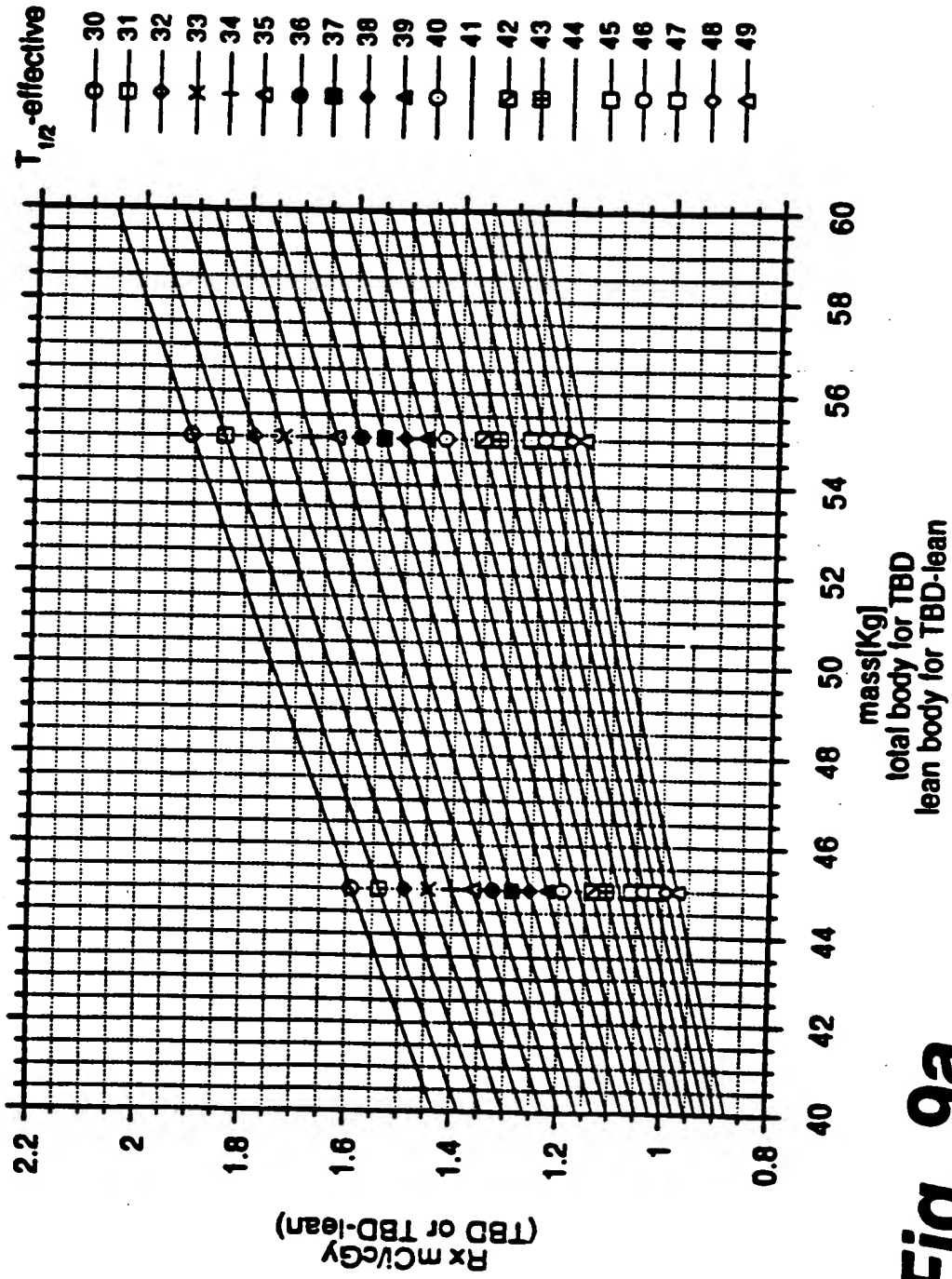
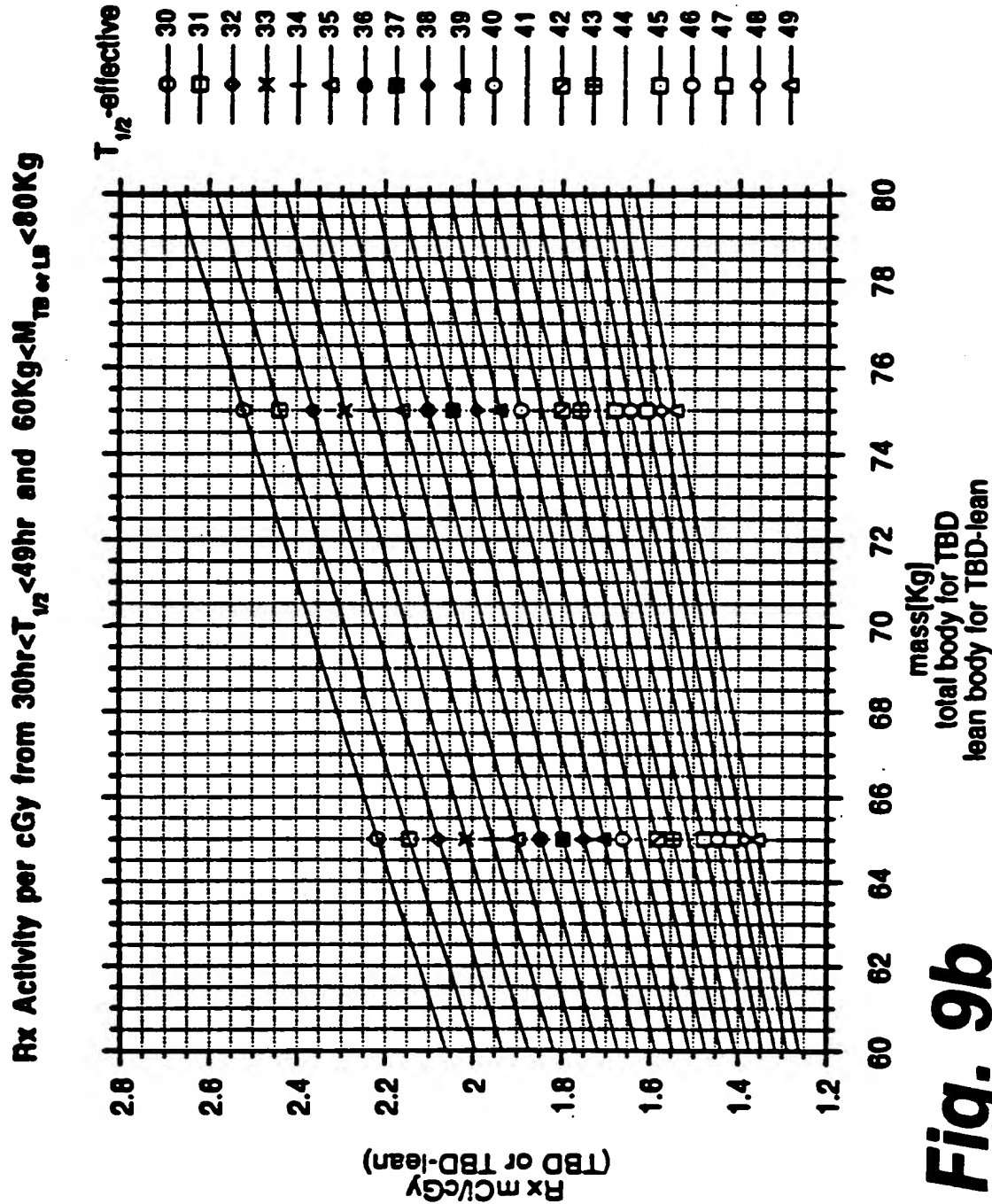


Fig. 9a

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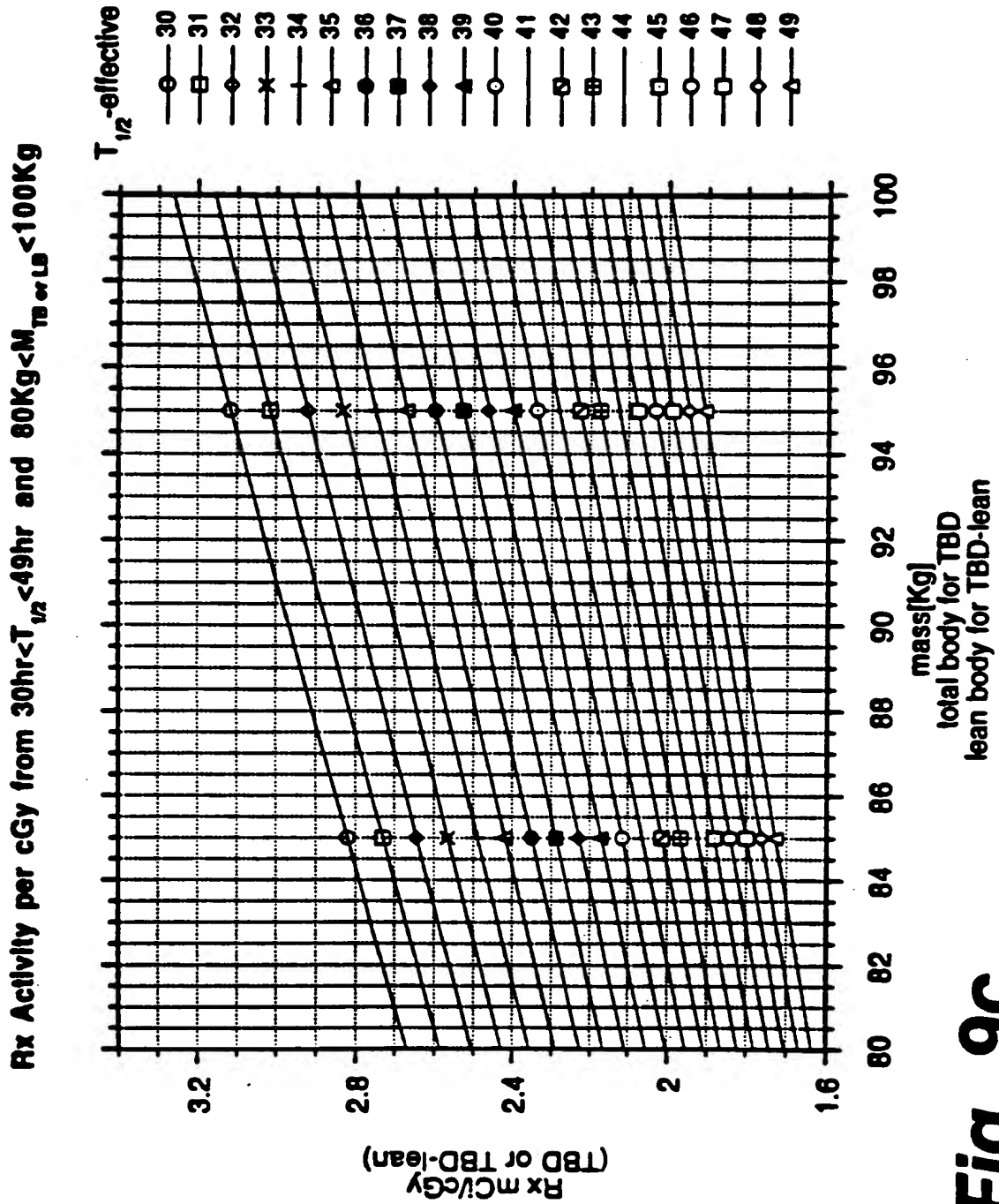


Fig. 9c

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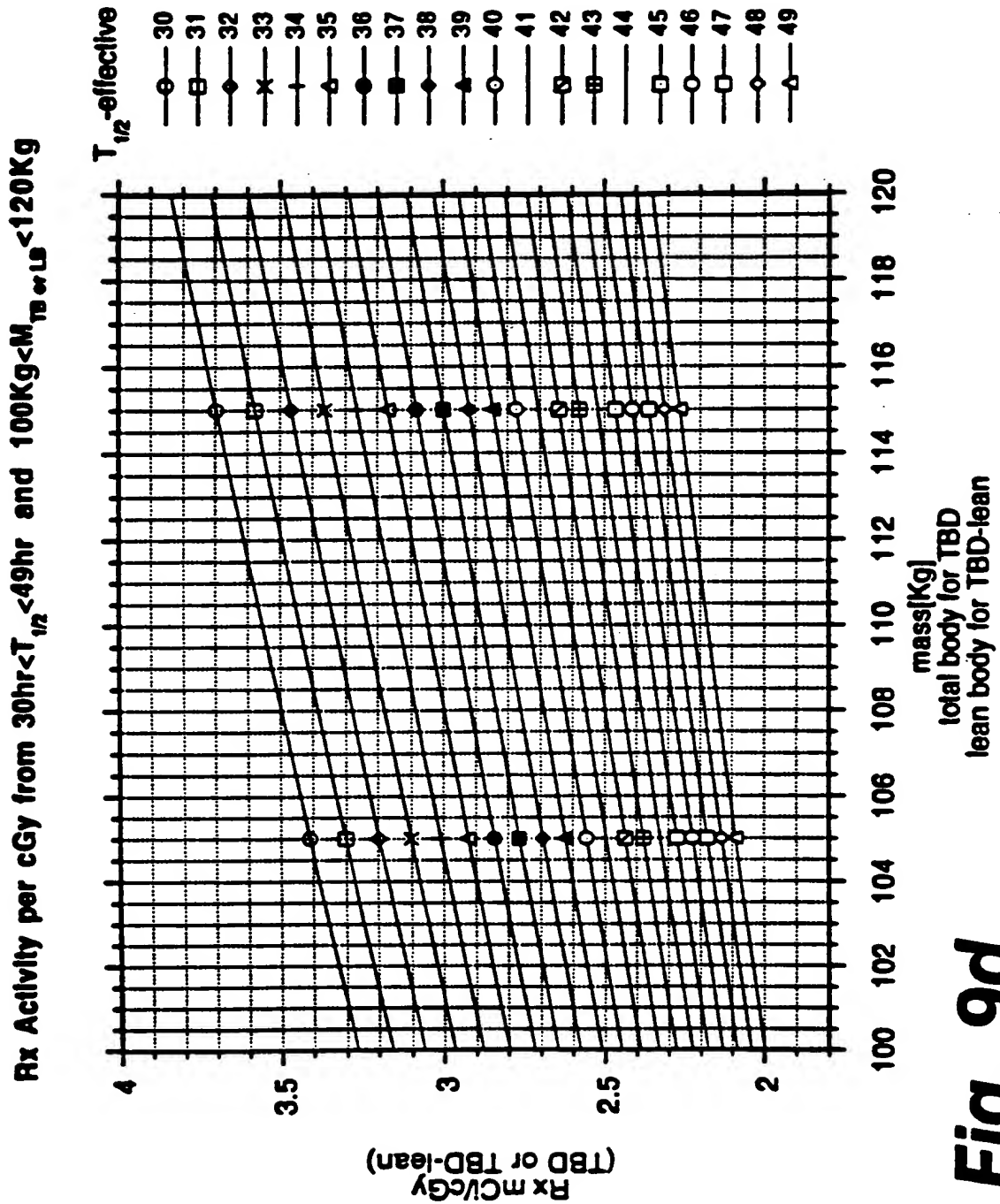


Fig. 9d

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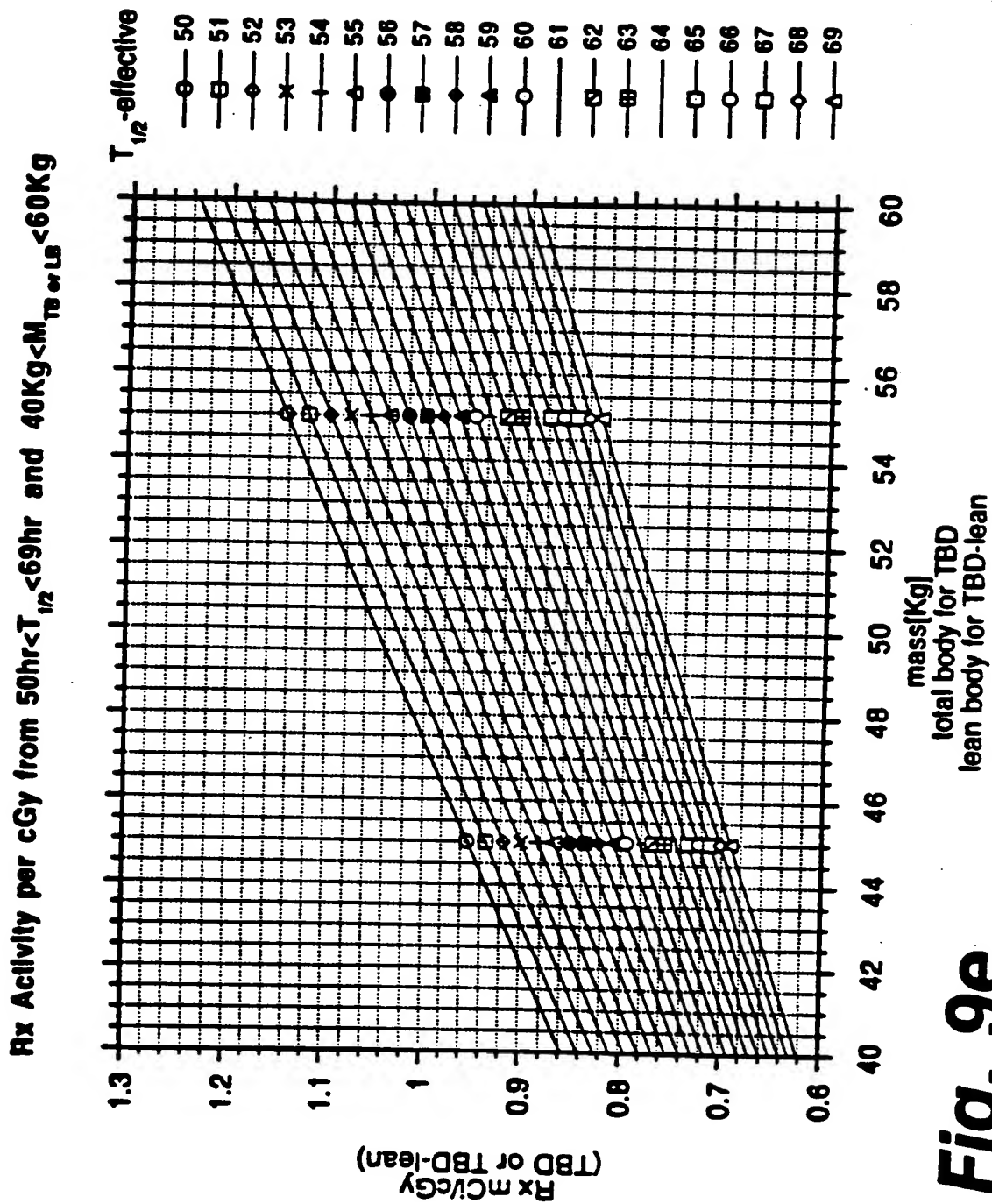
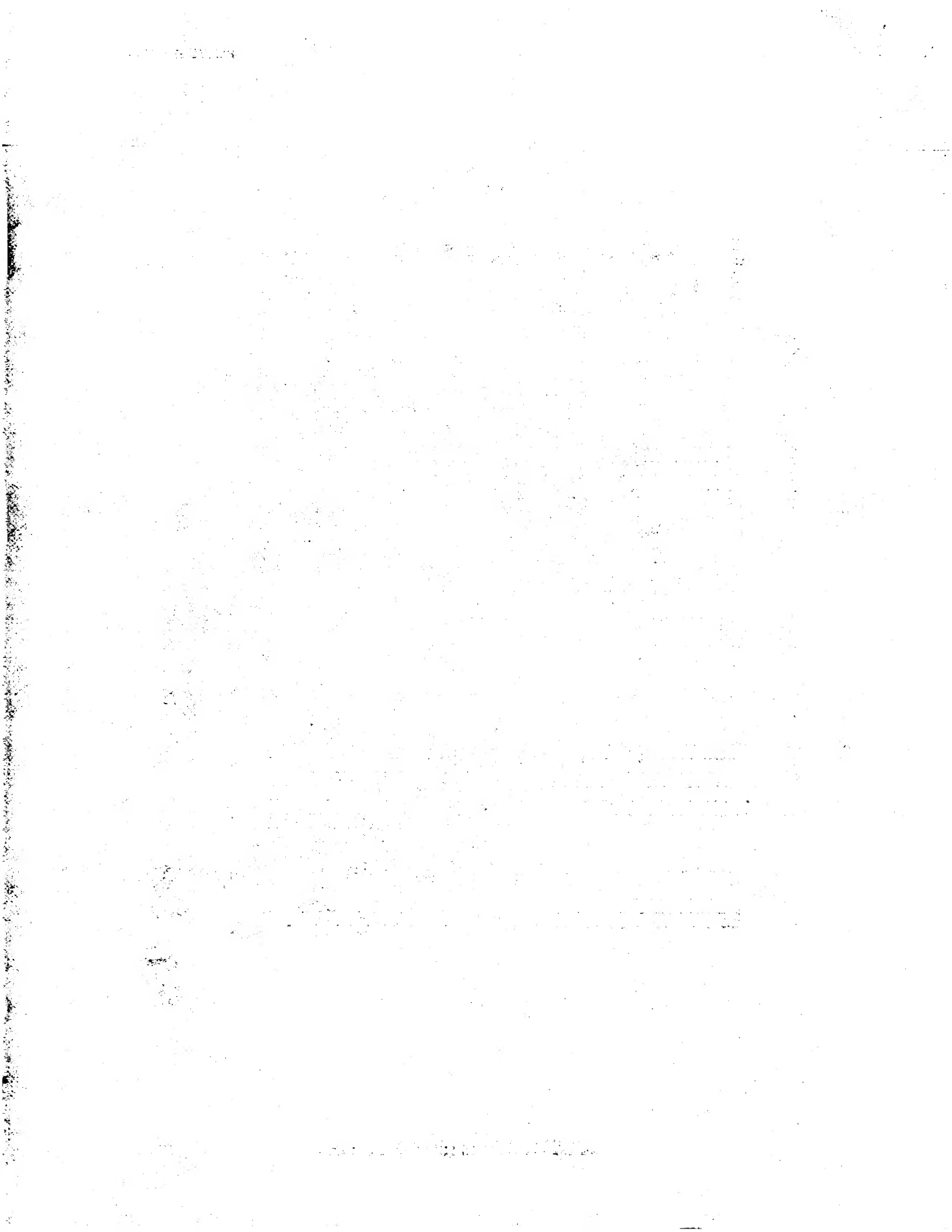


Fig. 9e



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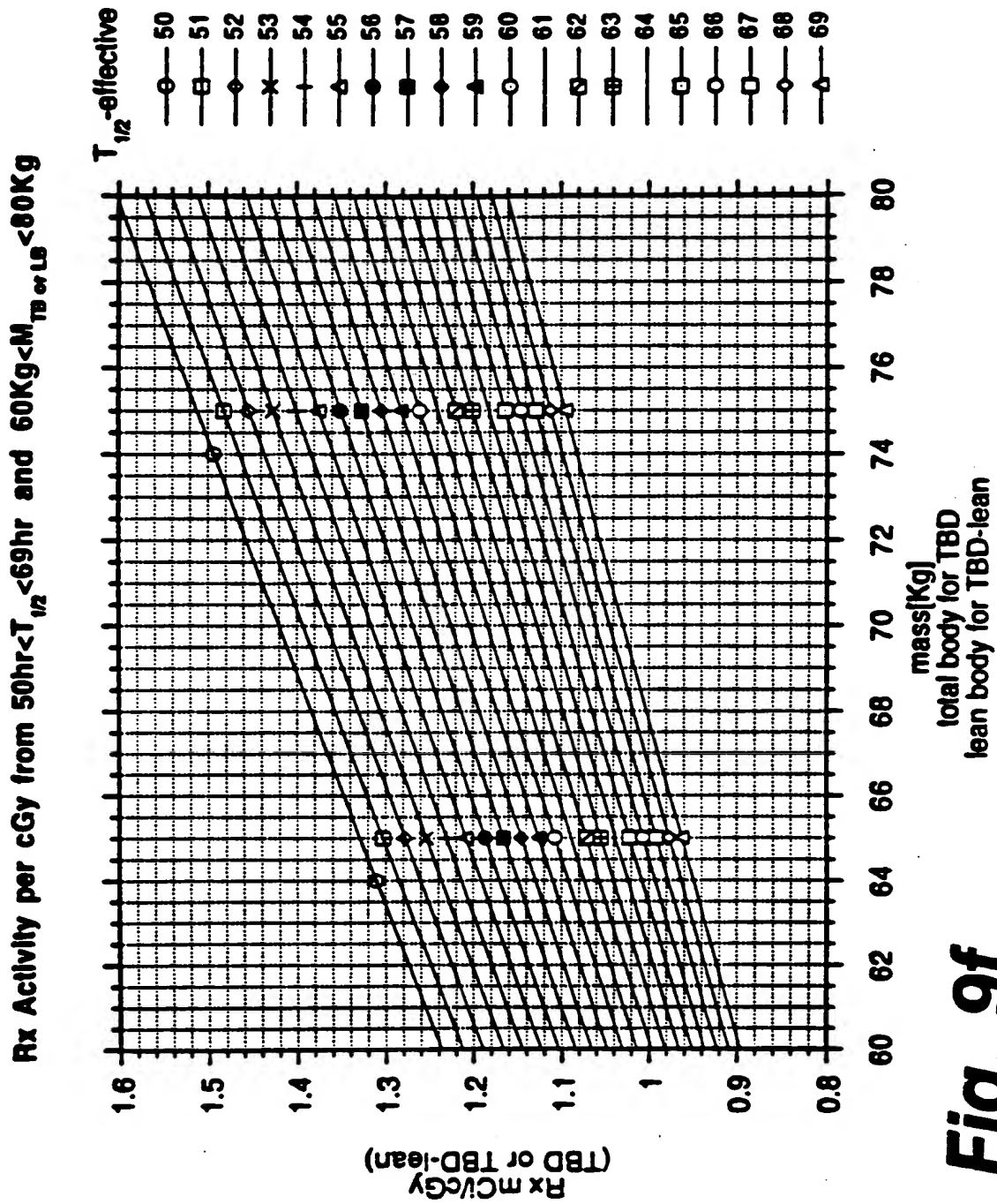


Fig. 9f

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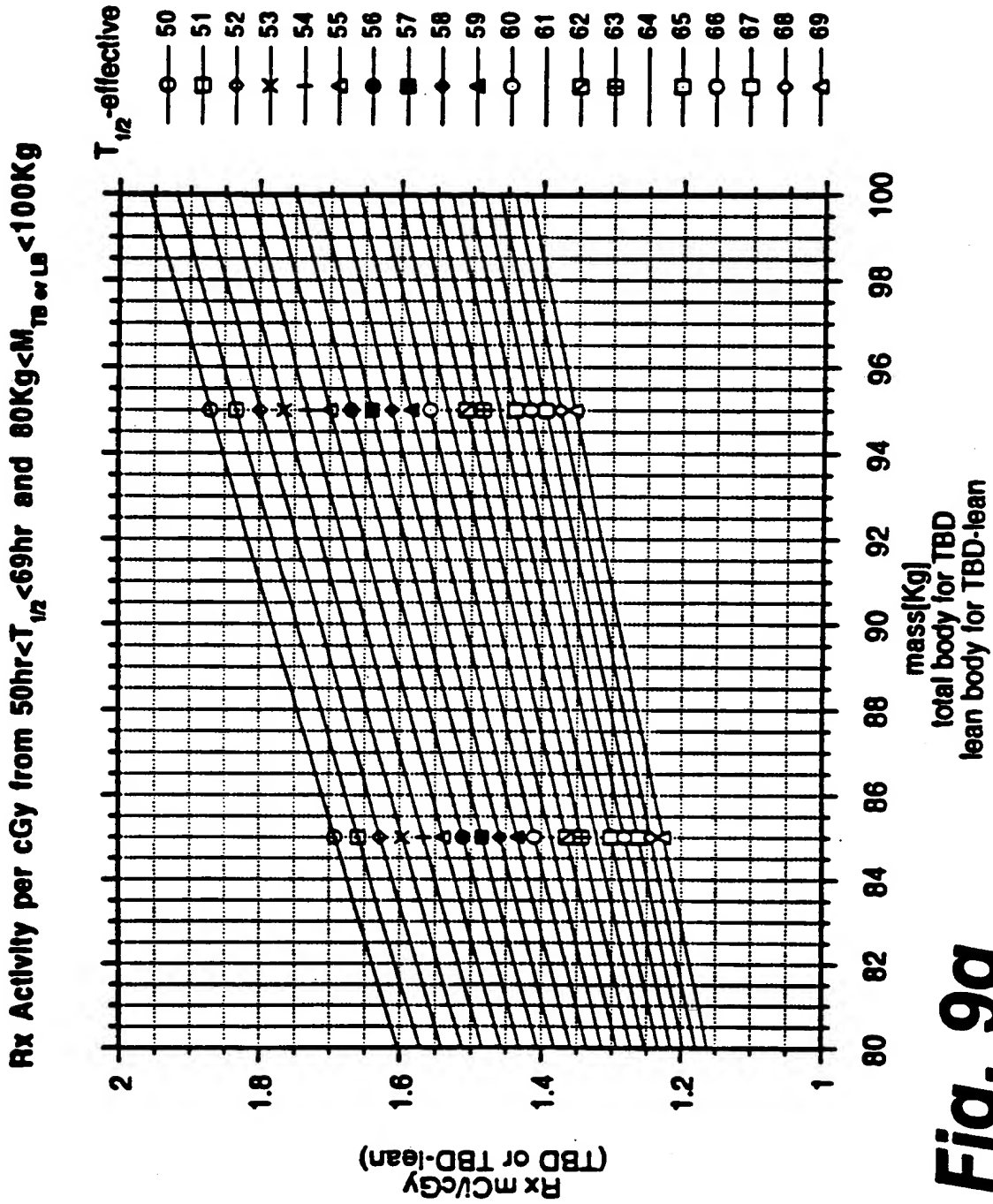


Fig. 9g

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Rx Activity per cGy from 50hr < $T_{1/2}$ < 69hr and 100Kg < M_{TB} or M_{LB} < 120Kg

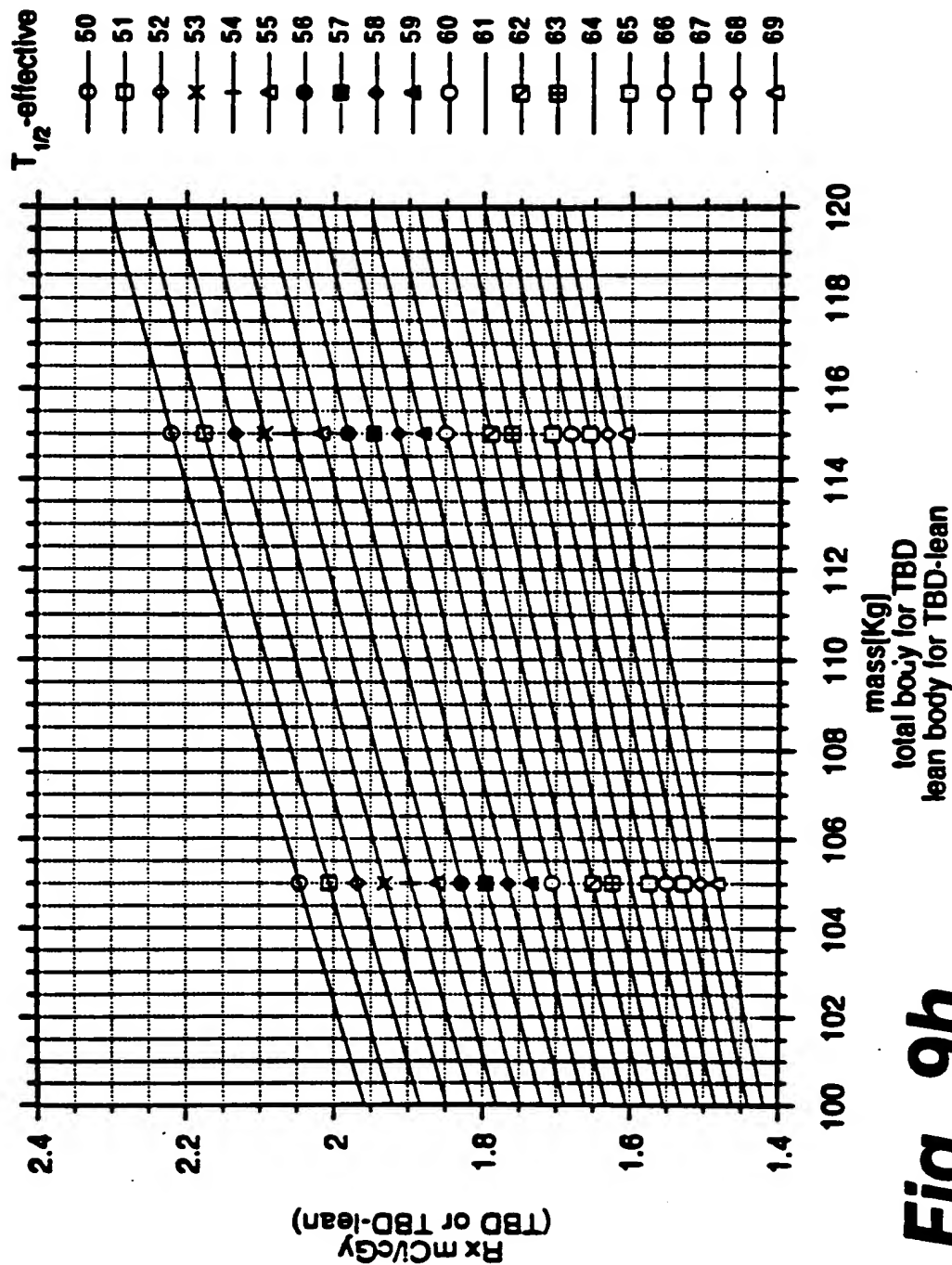


Fig. 9h

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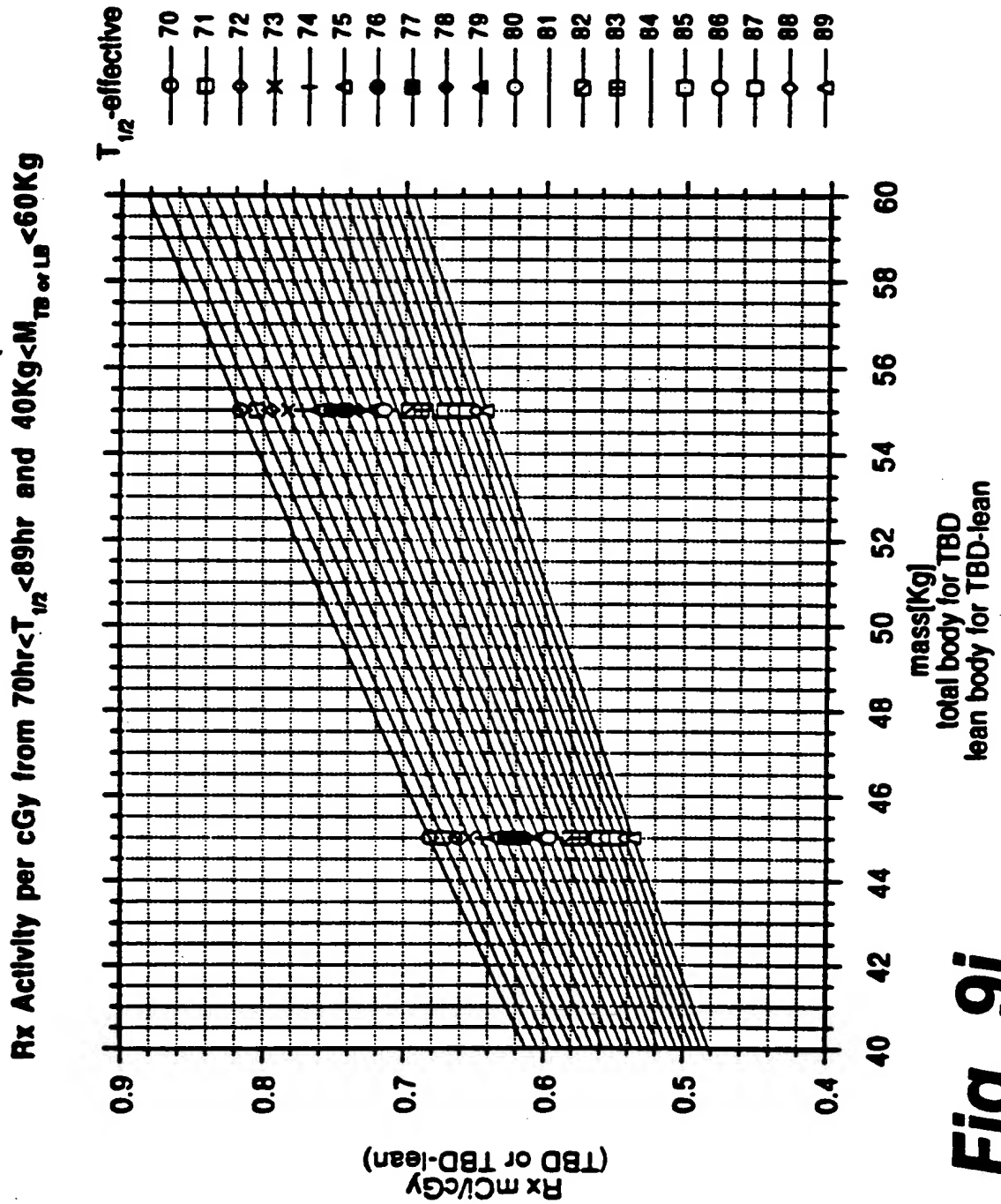


Fig. 9i

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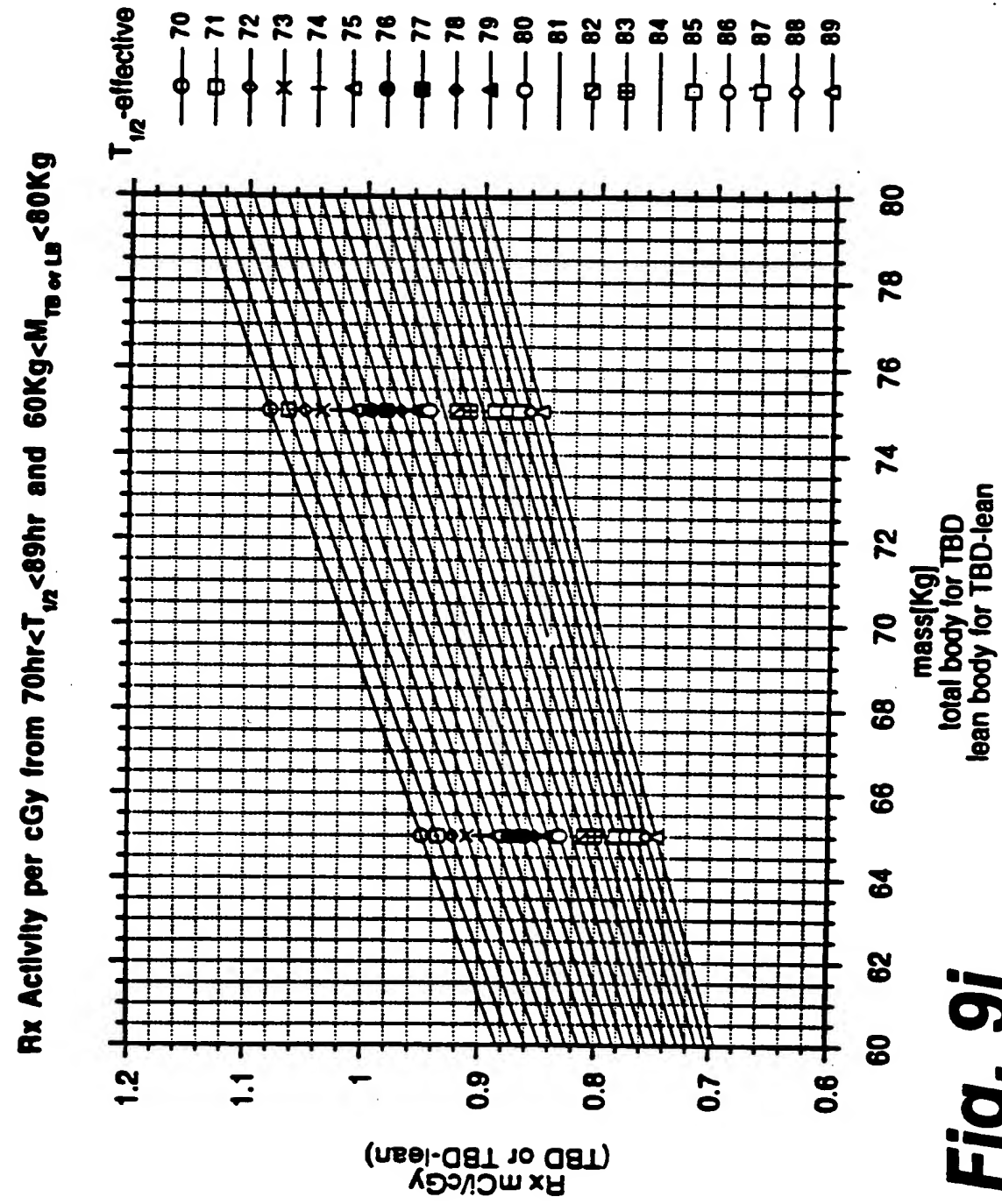
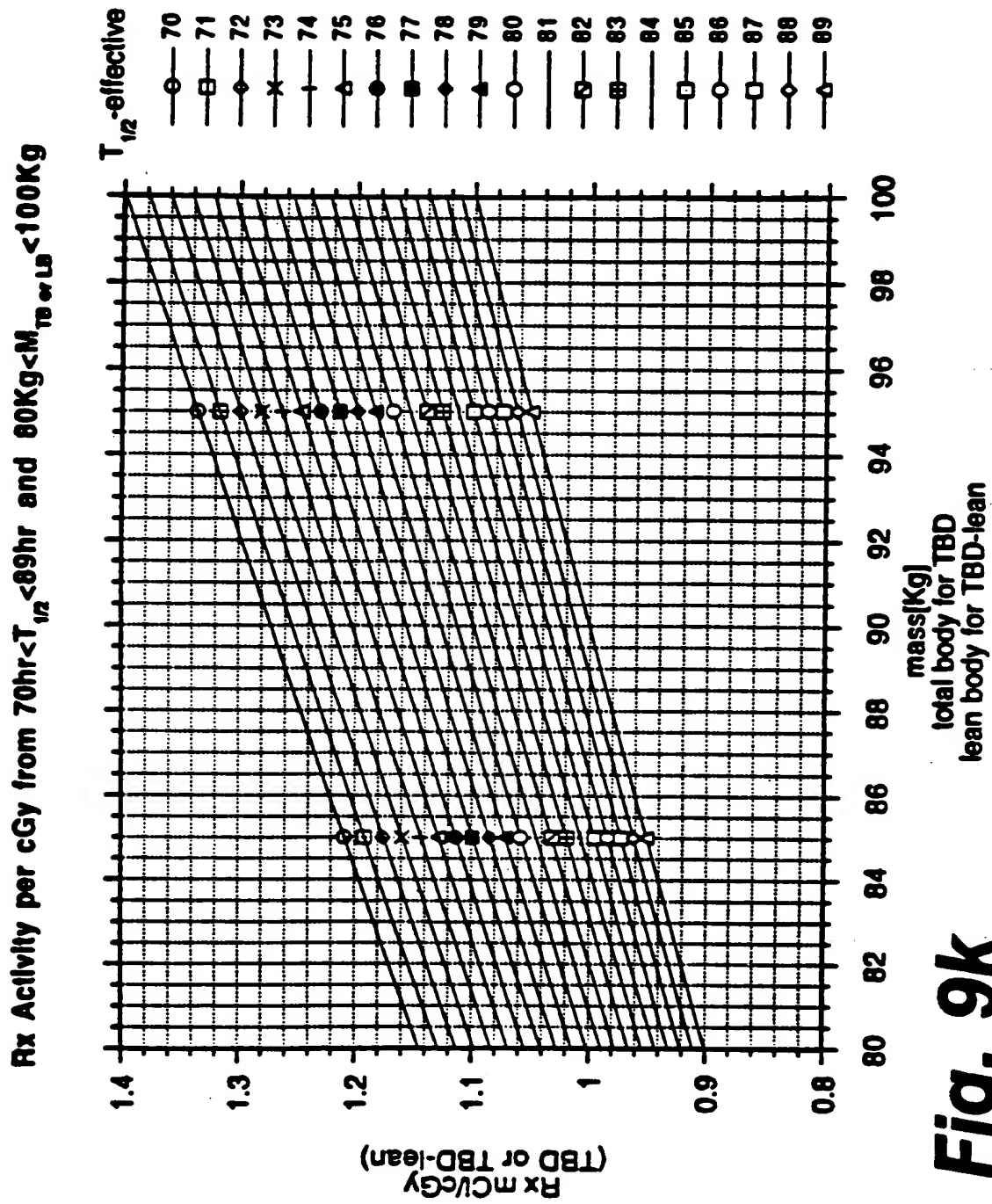


Fig. 9j

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Rx Activity per cGy from 70hr < $T_{1/2}$ < 89hr and 100Kg < $M_{TB \text{ or } LB}$ < 120Kg

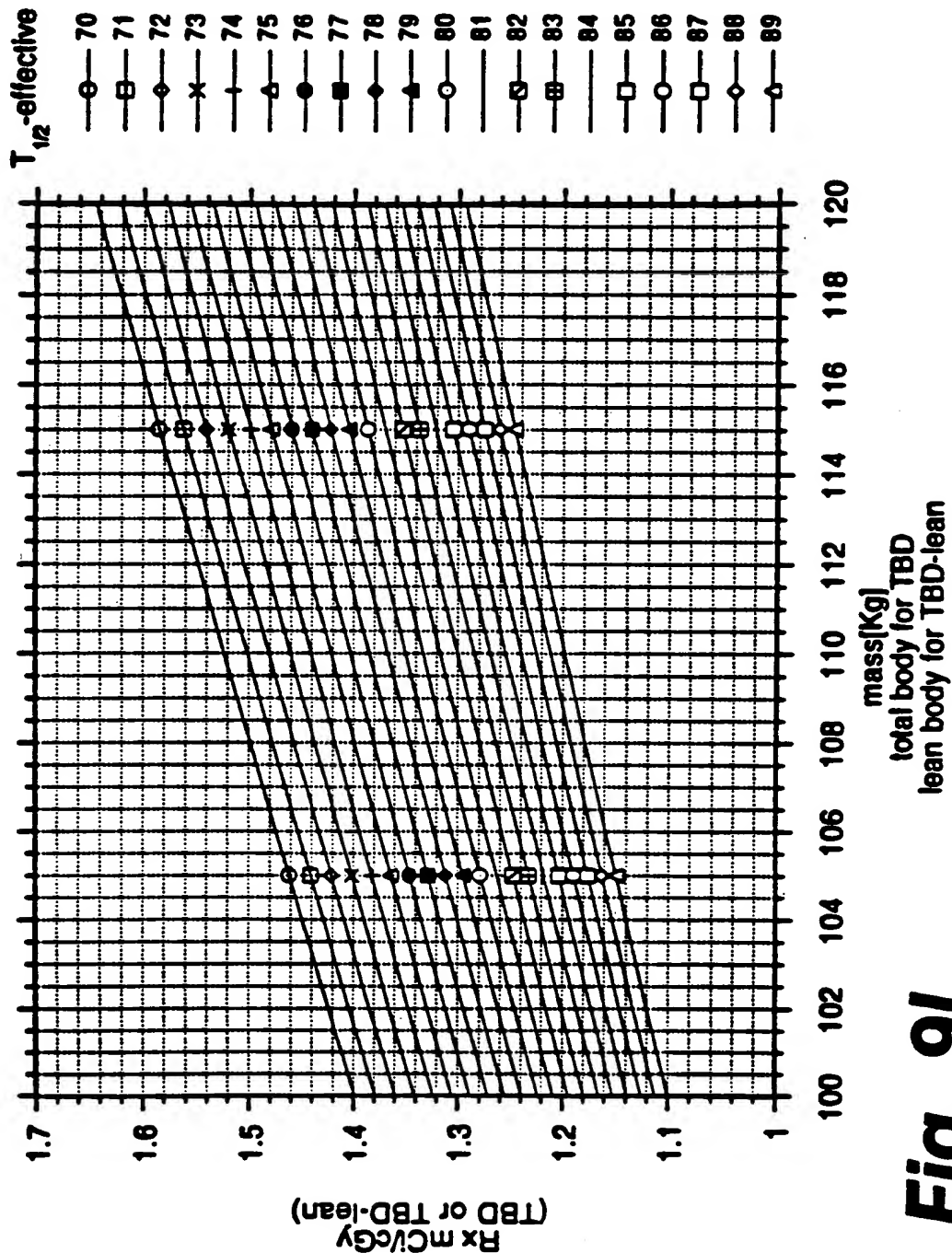


Fig. 91

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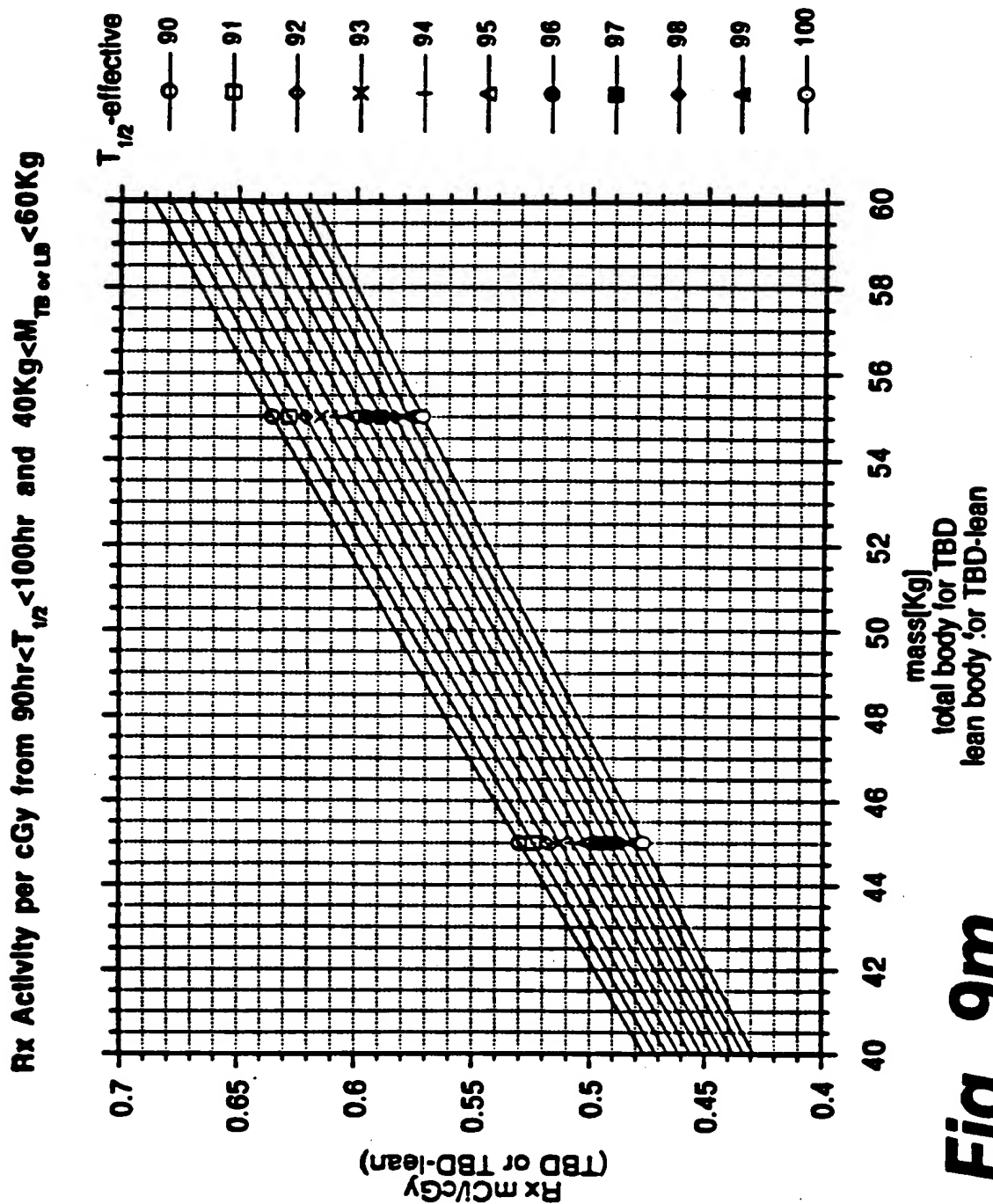


Fig. 9m

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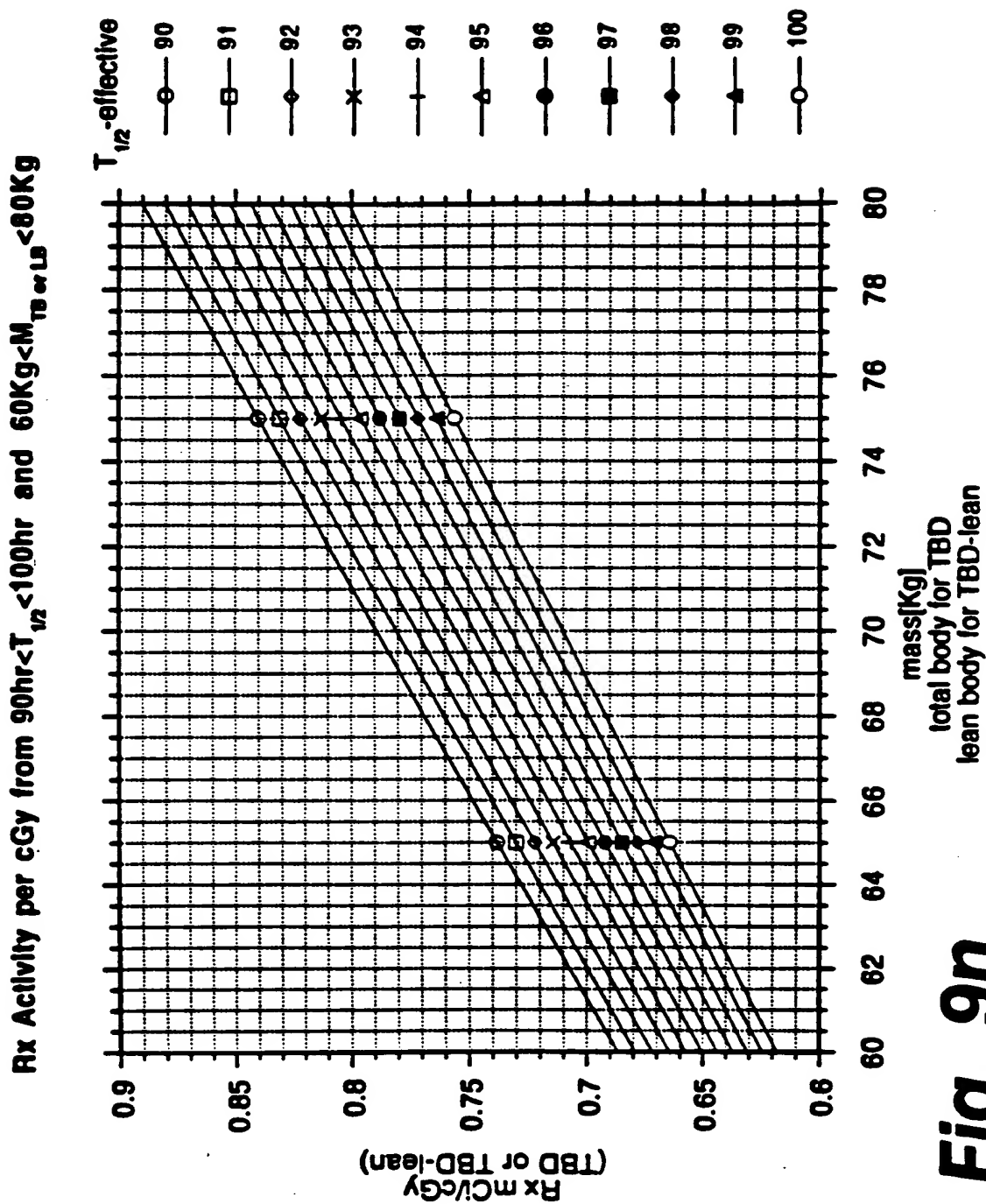


Fig. 9n

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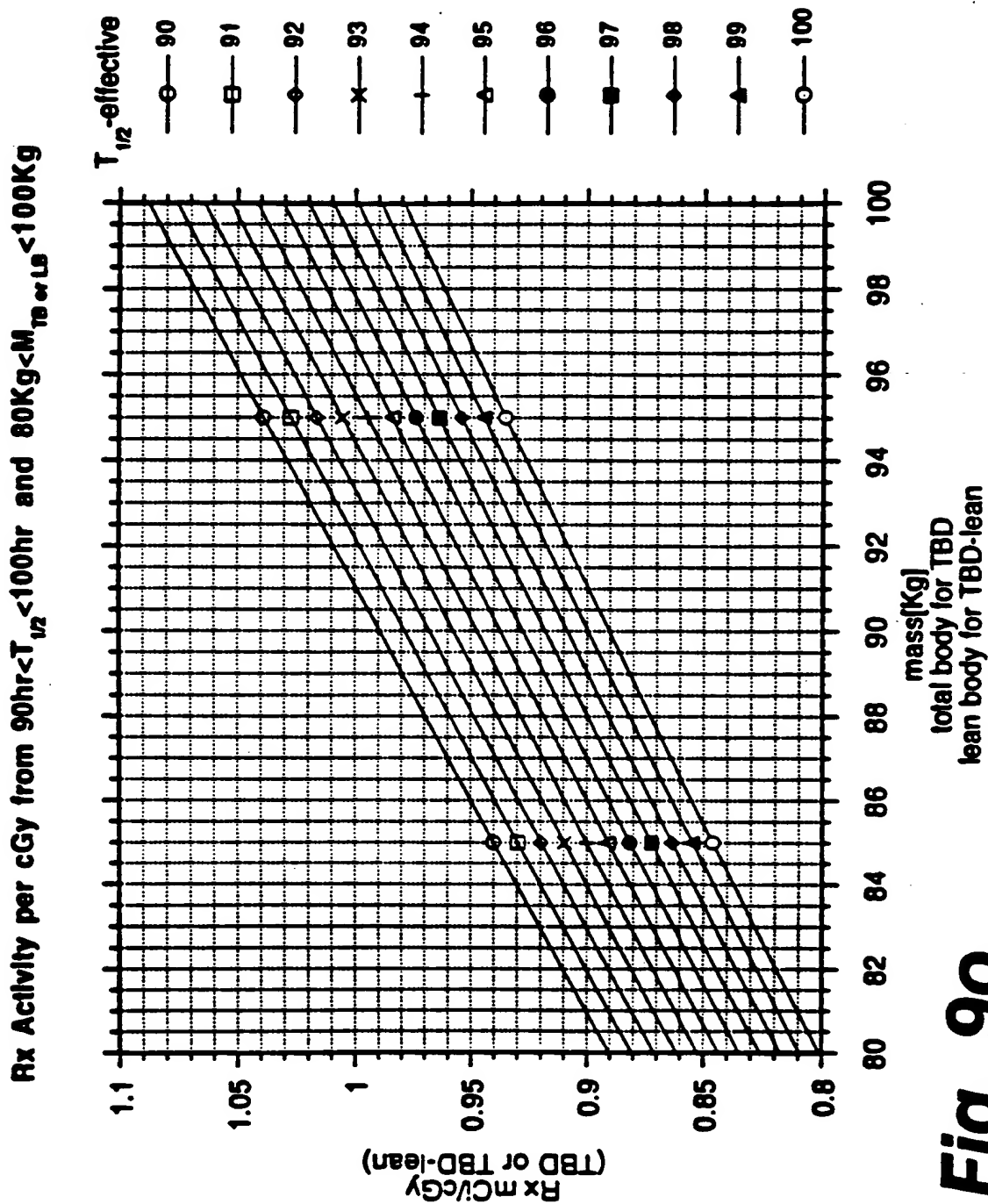


Fig. 90

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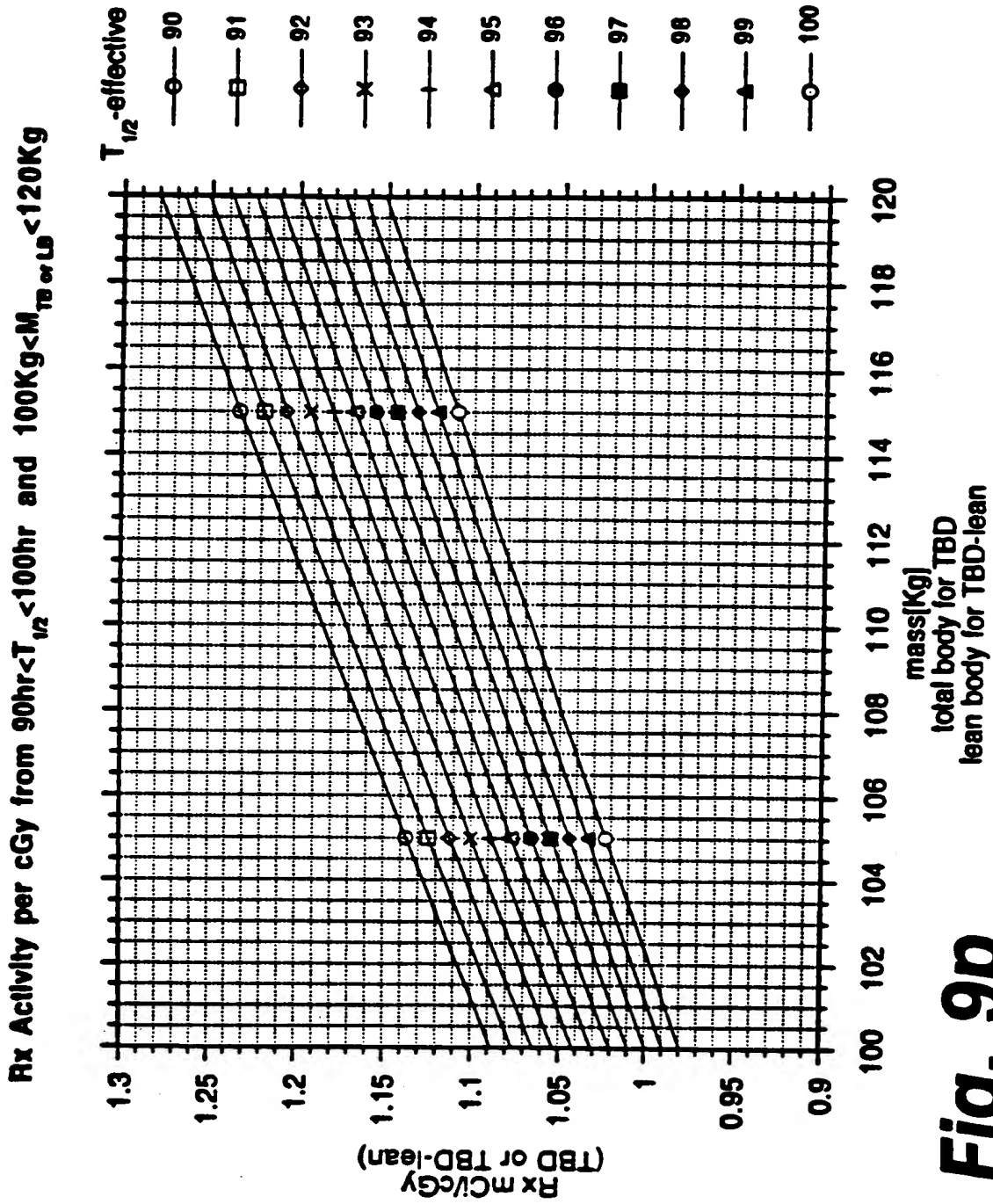


Fig. 9p

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Fig. 10a

mCi per cGy results

Activity per unit Total Body Dose (TBD) or Less Body Dose (LBD-Lean) as a function of Total Body or Less body mass and TMS-effective

LBM estimates from:

Female: $LBM = 48.9 + 0.01 \cdot (HT - 152)$ [HT in cm, LBM in Kg]Male: $LBM = 48.0 + 1.08 \cdot (HT - 152)$ Total Body mass for Total Body dose
Less Body mass (LBM) for Total Body Dose-Lean

V	T-1/2(t)-effective →										A0 [mChGdV]										
mass (kg)	30	31	32	33	34	35	36	37	38	39	40	41	42	43	44	45	46	47	48	49	50
40	1.426	1.393	1.359	1.326	1.291	1.256	1.221	1.186	1.151	1.116	1.081	1.046	1.011	0.976	0.941	0.906	0.871	0.836	0.801	0.766	0.731
41	1.481	1.446	1.411	1.376	1.341	1.306	1.271	1.236	1.201	1.166	1.131	1.096	1.061	1.026	0.991	0.956	0.921	0.886	0.851	0.816	0.781
42	1.493	1.448	1.403	1.357	1.312	1.267	1.222	1.177	1.132	1.087	1.042	0.997	0.952	0.907	0.862	0.817	0.772	0.727	0.682	0.637	0.592
43	1.526	1.476	1.430	1.387	1.346	1.307	1.271	1.237	1.204	1.173	1.144	1.116	1.086	1.064	1.040	1.017	0.988	0.874	0.863	0.834	0.815
44	1.537	1.507	1.480	1.418	1.374	1.335	1.296	1.263	1.228	1.198	1.168	1.138	1.108	1.080	1.042	1.036	1.016	0.864	0.873	0.853	0.834
45	1.588	1.538	1.490	1.448	1.402	1.362	1.324	1.286	1.255	1.222	1.192	1.163	1.135	1.109	1.093	1.059	1.036	1.014	0.993	0.973	0.953
46	1.621	1.569	1.520	1.474	1.430	1.387	1.351	1.314	1.280	1.247	1.216	1.186	1.156	1.131	1.105	1.081	1.057	1.035	1.013	0.992	0.972
47	1.653	1.599	1.549	1.502	1.458	1.417	1.377	1.340	1.305	1.271	1.239	1.209	1.180	1.153	1.127	1.102	1.078	1.055	1.033	1.012	0.992
48	1.684	1.630	1.579	1.531	1.486	1.444	1.404	1.366	1.330	1.296	1.263	1.232	1.203	1.176	1.146	1.123	1.099	1.075	1.053	1.031	1.011
49	1.716	1.661	1.609	1.560	1.514	1.471	1.430	1.391	1.355	1.324	1.311	1.279	1.248	1.219	1.191	1.165	1.140	1.115	1.088	1.072	1.051
50	1.747	1.691	1.638	1.586	1.542	1.498	1.456	1.417	1.380	1.344	1.311	1.278	1.246	1.216	1.188	1.161	1.136	1.110	1.082	1.070	1.046
51	1.778	1.722	1.668	1.617	1.570	1.526	1.482	1.442	1.404	1.368	1.334	1.302	1.271	1.241	1.213	1.186	1.160	1.136	1.118	1.098	1.067
52	1.812	1.752	1.697	1.646	1.597	1.552	1.509	1.468	1.429	1.393	1.358	1.326	1.293	1.263	1.234	1.207	1.181	1.156	1.138	1.118	1.086
53	1.842	1.782	1.727	1.674	1.625	1.576	1.535	1.493	1.454	1.417	1.381	1.346	1.316	1.285	1.256	1.228	1.201	1.176	1.151	1.128	1.105
54	1.873	1.813	1.758	1.703	1.653	1.608	1.561	1.516	1.478	1.441	1.405	1.371	1.336	1.307	1.277	1.246	1.222	1.198	1.171	1.147	1.124
55	1.904	1.843	1.785	1.731	1.680	1.632	1.587	1.544	1.503	1.463	1.426	1.393	1.360	1.329	1.296	1.270	1.242	1.216	1.190	1.166	1.143
56	1.936	1.873	1.815	1.760	1.708	1.658	1.613	1.569	1.528	1.488	1.452	1.416	1.383	1.350	1.320	1.290	1.262	1.236	1.210	1.185	1.161
57	1.967	1.903	1.844	1.788	1.735	1.686	1.639	1.593	1.553	1.513	1.478	1.439	1.405	1.372	1.341	1.311	1.283	1.256	1.229	1.204	1.180
58	1.999	1.933	1.873	1.816	1.763	1.712	1.665	1.620	1.577	1.537	1.498	1.462	1.427	1.394	1.362	1.332	1.303	1.276	1.249	1.223	1.199
59	2.030	1.963	1.902	1.844	1.790	1.738	1.691	1.645	1.602	1.561	1.522	1.485	1.446	1.416	1.393	1.353	1.323	1.296	1.269	1.242	1.217
60	2.060	1.993	1.931	1.873	1.818	1.766	1.717	1.670	1.626	1.585	1.545	1.507	1.471	1.437	1.404	1.373	1.343	1.316	1.287	1.261	1.236
61	2.091	2.023	1.960	1.901	1.845	1.792	1.742	1.695	1.651	1.608	1.568	1.530	1.493	1.459	1.426	1.394	1.364	1.335	1.307	1.280	1.254
62	2.122	2.053	1.990	1.929	1.872	1.816	1.764	1.720	1.675	1.632	1.591	1.552	1.515	1.480	1.447	1.414	1.384	1.354	1.326	1.299	1.273
63	2.152	2.083	2.018	1.957	1.899	1.840	1.784	1.745	1.698	1.656	1.616	1.578	1.537	1.502	1.468	1.435	1.404	1.374	1.345	1.316	1.291
64	2.183	2.113	2.047	1.985	1.926	1.871	1.819	1.770	1.724	1.679	1.637	1.597	1.556	1.523	1.488	1.455	1.424	1.394	1.364	1.337	1.310
65	2.214	2.143	2.078	2.015	1.953	1.896	1.845	1.796	1.748	1.703	1.660	1.620	1.580	1.545	1.509	1.479	1.444	1.413	1.384	1.355	1.326
66	2.245	2.172	2.104	2.040	1.980	1.924	1.870	1.820	1.772	1.727	1.683	1.642	1.603	1.563	1.526	1.488	1.454	1.423	1.393	1.374	1.347
67	2.275	2.202	2.133	2.068	2.008	1.950	1.896	1.845	1.796	1.750	1.706	1.665	1.626	1.587	1.551	1.517	1.484	1.452	1.422	1.393	1.367
68	2.306	2.231	2.162	2.096	2.036	1.976	1.922	1.870	1.820	1.774	1.730	1.687	1.647	1.609	1.572	1.539	1.506	1.474	1.442	1.412	1.385
69	2.336	2.261	2.191	2.124	2.062	2.002	1.947	1.894	1.842	1.797	1.753	1.710	1.669	1.630	1.593	1.559	1.526	1.494	1.462	1.432	1.405
70	2.367	2.291	2.219	2.152	2.089	2.029	1.972	1.916	1.869	1.821	1.776	1.732	1.689	1.650	1.613	1.579	1.546	1.514	1.482	1.451	1.423
71	2.398	2.320	2.248	2.180	2.115	2.055	1.998	1.944	1.893	1.844	1.794	1.754	1.713	1.675	1.639	1.605	1.572	1.540	1.511	1.479	1.448
72	2.428	2.350	2.278	2.209	2.142	2.081	2.023	1.969	1.917	1.868	1.821	1.777	1.736	1.694	1.658	1.624	1.591	1.560	1.530	1.498	1.468
73	2.458	2.379	2.305	2.235	2.168	2.107	2.049	1.993	1.941	1.891	1.844	1.798	1.756	1.715	1.676	1.638	1.603	1.569	1.536	1.505	1.475
74	2.488	2.409	2.333	2.263	2.196	2.133	2.074	2.018	1.965	1.915	1.867	1.821	1.778	1.737	1.697	1.658	1.623	1.589	1.557	1.526	1.495
75	2.520	2.438	2.362	2.292	2.225	2.160	2.100	2.043	1.989	1.938	1.890	1.844	1.800	1.759	1.719	1.680	1.643	1.608	1.576	1.545	1.514
76	2.550	2.468	2.391	2.318	2.250	2.186	2.125	2.067	2.013	1.961	1.912	1.864	1.821	1.779	1.739	1.700	1.663	1.628	1.594	1.561	1.530
77	2.580	2.497	2.418	2.349	2.277	2.212	2.150	2.092	2.037	1.985	1.935	1.886	1.843	1.800	1.759	1.720	1.683	1.648	1.613	1.580	1.548
78	2.610	2.526	2.447	2.373	2.303	2.236	2.175	2.117	2.061	2.009	1.958	1.908	1.863	1.821	1.780	1.740	1.702	1.666	1.632	1.598	1.566
79	2.641	2.555	2.476	2.401	2.330	2.263	2.201	2.141	2.085	2.031	1.980	1.932	1.889	1.847	1.806	1.766	1.728	1.692	1.658	1.624	1.592
80	2.671	2.585	2.504	2.428	2.357	2.288	2.226	2.165	2.108	2.054	2.003	1.954	1.908	1.863	1.821	1.780	1.742	1.705	1.669	1.635	1.602
81	2.701	2.614	2.532	2.455	2.383	2.316	2.251	2.189	2.130	2.074	2.020	1.970	1.924	1.881	1.841	1.800	1.761	1.724	1.689	1.655	1.620
82	2.731	2.642	2.560	2.482	2.409	2.340	2.276	2.214	2.156	2.100	2.046	1.994	1.950	1.908	1.867	1.826	1.787	1.750	1.715	1.681	1.646
83	2.760	2.671	2.588	2.509	2.436	2.368	2.300	2.236	2.178	2.123	2.070	2.020	1.976	1.934	1.892	1.850	1.810	1.772	1.737	1.702	1.667

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Fig. 10b

mCi per cGy matrix

Total Rod Lead Rod	V	T _{1/2} (hr)-effective →	51	52	53	54	55	56	57	58	59	60	61	62	63	64	65	66	67	68	69	70	71
40	0.840	0.824	0.809	0.794	0.779	0.765	0.752	0.739	0.728	0.714	0.703	0.691	0.680	0.670	0.658	0.646	0.635	0.624	0.614	0.603	0.592	0.581	0.571
41	0.856	0.843	0.827	0.812	0.797	0.783	0.769	0.756	0.743	0.730	0.716	0.707	0.696	0.685	0.674	0.664	0.653	0.642	0.632	0.621	0.611	0.601	0.591
42	0.878	0.861	0.845	0.829	0.814	0.800	0.786	0.772	0.758	0.747	0.734	0.722	0.711	0.700	0.689	0.678	0.667	0.656	0.645	0.634	0.624	0.613	0.603
43	0.897	0.880	0.863	0.847	0.832	0.817	0.803	0.789	0.776	0.763	0.750	0.738	0.726	0.715	0.704	0.693	0.682	0.671	0.660	0.649	0.638	0.627	0.616
44	0.910	0.893	0.876	0.860	0.845	0.830	0.816	0.802	0.788	0.776	0.763	0.751	0.740	0.729	0.718	0.707	0.696	0.685	0.674	0.663	0.652	0.641	0.630
45	0.928	0.911	0.894	0.878	0.863	0.848	0.834	0.820	0.806	0.792	0.780	0.768	0.757	0.746	0.735	0.724	0.713	0.702	0.691	0.680	0.669	0.658	0.647
46	0.953	0.935	0.917	0.900	0.884	0.868	0.853	0.839	0.824	0.810	0.797	0.784	0.772	0.760	0.748	0.737	0.726	0.715	0.704	0.693	0.682	0.671	0.660
47	0.972	0.953	0.935	0.918	0.901	0.885	0.870	0.855	0.840	0.826	0.813	0.800	0.787	0.775	0.763	0.751	0.740	0.729	0.718	0.707	0.696	0.685	0.674
48	0.991	0.972	0.953	0.935	0.919	0.902	0.886	0.871	0.856	0.842	0.828	0.815	0.802	0.790	0.777	0.765	0.753	0.742	0.731	0.720	0.709	0.698	0.687
49	1.009	0.990	0.971	0.953	0.936	0.919	0.903	0.886	0.873	0.858	0.844	0.830	0.817	0.804	0.792	0.780	0.768	0.757	0.746	0.735	0.724	0.713	0.702
50	1.028	1.008	0.989	0.971	0.953	0.936	0.920	0.904	0.888	0.874	0.859	0.845	0.832	0.819	0.807	0.794	0.782	0.771	0.760	0.749	0.738	0.727	0.716
51	1.046	1.026	1.007	0.989	0.970	0.953	0.936	0.920	0.904	0.888	0.874	0.859	0.845	0.832	0.819	0.807	0.794	0.782	0.771	0.760	0.749	0.738	0.727
52	1.063	1.043	1.023	1.005	0.987	0.968	0.951	0.934	0.917	0.901	0.885	0.870	0.855	0.842	0.829	0.816	0.804	0.792	0.781	0.770	0.759	0.748	0.737
53	1.082	1.061	1.040	1.021	1.003	0.984	0.966	0.948	0.931	0.914	0.897	0.881	0.865	0.849	0.833	0.817	0.801	0.785	0.769	0.753	0.737	0.721	0.705
54	1.102	1.081	1.059	1.039	1.019	1.000	0.981	0.962	0.944	0.926	0.908	0.891	0.874	0.857	0.840	0.823	0.806	0.790	0.774	0.758	0.742	0.726	0.710
55	1.120	1.098	1.076	1.055	1.034	1.014	0.994	0.974	0.954	0.934	0.914	0.894	0.874	0.854	0.834	0.814	0.794	0.774	0.754	0.734	0.714	0.694	0.674
56	1.137	1.115	1.093	1.071	1.049	1.027	1.005	0.983	0.961	0.939	0.917	0.895	0.873	0.851	0.829	0.807	0.785	0.763	0.741	0.719	0.697	0.675	0.653
57	1.155	1.131	1.108	1.085	1.062	1.039	1.016	0.993	0.969	0.946	0.923	0.900	0.877	0.854	0.831	0.808	0.785	0.762	0.739	0.716	0.693	0.670	0.647
58	1.173	1.148	1.124	1.100	1.076	1.052	1.028	1.004	0.980	0.956	0.932	0.908	0.884	0.860	0.836	0.812	0.788	0.764	0.740	0.716	0.692	0.668	0.644
59	1.191	1.165	1.140	1.115	1.090	1.065	1.040	1.015	0.990	0.965	0.940	0.915	0.890	0.865	0.840	0.815	0.790	0.765	0.740	0.715	0.690	0.665	0.640
60	1.210	1.183	1.157	1.131	1.105	1.079	1.053	1.027	1.001	0.975	0.949	0.923	0.897	0.871	0.845	0.819	0.793	0.767	0.741	0.715	0.689	0.663	0.637
61	1.230	1.202	1.175	1.148	1.121	1.094	1.067	1.040	1.013	0.986	0.959	0.932	0.905	0.878	0.851	0.824	0.797	0.770	0.743	0.716	0.689	0.662	0.635
62	1.248	1.220	1.192	1.164	1.136	1.108	1.080	1.052	1.024	0.996	0.968	0.940	0.912	0.884	0.856	0.828	0.800	0.772	0.744	0.716	0.688	0.660	0.632
63	1.266	1.237	1.208	1.179	1.150	1.121	1.092	1.063	1.034	1.005	0.976	0.947	0.918	0.889	0.860	0.831	0.802	0.773	0.744	0.715	0.686	0.657	0.628
64	1.284	1.255	1.225	1.195	1.165	1.135	1.105	1.075	1.045	1.015	0.985	0.955	0.925	0.895	0.865	0.835	0.805	0.775	0.745	0.715	0.685	0.655	0.625
65	1.302	1.272	1.242	1.211	1.180	1.149	1.118	1.087	1.056	1.025	0.994	0.963	0.932	0.901	0.870	0.839	0.808	0.777	0.746	0.715	0.684	0.653	0.622
66	1.320	1.289	1.258	1.226	1.194	1.162	1.130	1.098	1.066	1.034	1.002	0.970	0.938	0.906	0.874	0.842	0.810	0.778	0.746	0.714	0.682	0.650	0.618
67	1.338	1.306	1.274	1.241	1.208	1.175	1.142	1.109	1.076	1.043	1.010	0.977	0.944	0.911	0.878	0.845	0.812	0.779	0.746	0.713	0.680	0.647	0.614
68	1.356	1.323	1.290	1.256	1.222	1.188	1.154	1.120	1.086	1.052	1.018	0.984	0.950	0.916	0.882	0.848	0.814	0.780	0.746	0.712	0.678	0.644	0.610
69	1.374	1.340	1.306	1.271	1.236	1.201	1.166	1.131	1.096	1.061	1.026	0.991	0.956	0.921	0.886	0.851	0.816	0.781	0.746	0.711	0.676	0.641	0.606
70	1.392	1.357	1.322	1.286	1.250	1.214	1.178	1.142	1.106	1.070	1.034	0.998	0.962	0.926	0.890	0.854	0.818	0.782	0.746	0.710	0.674	0.638	0.602
71	1.410	1.375	1.338	1.301	1.264	1.227	1.190	1.153	1.116	1.079	1.042	1.005	0.968	0.931	0.894	0.857	0.820	0.783	0.746	0.709	0.672	0.635	0.598
72	1.428	1.401	1.374	1.346	1.324	1.301	1.278	1.255	1.232	1.209	1.186	1.163	1.140	1.117	1.094	1.071	1.048	1.025	1.002	0.979	0.956	0.933	0.910
73	1.446	1.418	1.391	1.362	1.341	1.317	1.294	1.272	1.250	1.228	1.205	1.183	1.160	1.138	1.115	1.093	1.070	1.047	1.024	1.001	0.978	0.955	0.932
74	1.464	1.436	1.409	1.383	1.356	1.333	1.310	1.287	1.264	1.241	1.218	1.195	1.172	1.149	1.126	1.103	1.080	1.057	1.034	1.011	0.988	0.965	0.942
75	1.482	1.454	1.428	1.400	1.374	1.350	1.326	1.303	1.280	1.257	1.234	1.211	1.188	1.165	1.142	1.119	1.096	1.073	1.050	1.027	1.004	0.981	0.958
76	1.500	1.471	1.445	1.417	1.391	1.366	1.342	1.318	1.294	1.270	1.246	1.222	1.198	1.174	1.150	1.126	1.102	1.078	1.054	1.030	1.006	0.982	0.958
77	1.518	1.488	1.461	1.433	1.407	1.382	1.357	1.332	1.307	1.282	1.257	1.232	1.207	1.182	1.157	1.132	1.107	1.082	1.057	1.032	1.007	0.982	0.957
78	1.536	1.506	1.478	1.450	1.424	1.398	1.373	1.347	1.321	1.295	1.269	1.243	1.217	1.191	1.165	1.139	1.113	1.087	1.061	1.035	1.009	0.983	0.957
79	1.553	1.523	1.495	1.467	1.440	1.414	1.388	1.362	1.336	1.310	1.284	1.258	1.232	1.206	1.180	1.154	1.128	1.102	1.076	1.050	1.024	0.998	0.972
80	1.571	1.541	1.512	1.484	1.457	1.431	1.405	1.379	1.353	1.327	1.301	1.275	1.249	1.223	1.197	1.171	1.145	1.119	1.093	1.067	1.041	1.015	0.989
81	1.588	1.558	1.529	1.500	1.473	1.447	1.421	1.395	1.369	1.343	1.317	1.291	1.265	1.239	1.213	1.187	1.161	1.135	1.109	1.083	1.057	1.031	1.005
82	1.606	1.575	1.546	1.517	1.489	1.463	1.437	1.411	1.385	1.359	1.333	1.307	1.281	1.255	1.229	1.203	1.177	1.151	1.125	1.099	1.073	1.047	1.021
83	1.624	1.592	1.562	1.534	1.506	1.479	1.453	1.427	1.401	1.375	1.349	1.323	1.297	1.271	1.245	1.219	1.193	1.167	1.141	1.115	1.089	1.063	1.037

25/35

Fig. 10c

mCi per cGy matrix

Total Rod Less Rod	V	T-1/2(T)-effective →										AO [mCi/cGy]																				
		72	73	74	75	76	77	78	79	80	81	82	83	84	85	86	87	88	89	90	91	92										
40	0.505	0.507	0.579	0.571	0.584	0.537	0.548	0.545	0.545	0.546	0.529	0.523	0.518	0.510	0.504	0.498	0.493	0.487	0.482	0.476	0.471	0.466										
41	0.508	0.500	0.502	0.504	0.577	0.589	0.542	0.555	0.546	0.541	0.534	0.528	0.522	0.516	0.510	0.504	0.498	0.492	0.487	0.482	0.476	0.471										
42	0.522	0.514	0.505	0.507	0.508	0.502	0.574	0.507	0.500	0.553	0.540	0.540	0.533	0.527	0.521	0.515	0.509	0.503	0.498	0.492	0.487	0.482										
43	0.535	0.527	0.518	0.510	0.502	0.504	0.507	0.579	0.507	0.556	0.543	0.540	0.533	0.527	0.521	0.515	0.509	0.503	0.498	0.492	0.487	0.482										
44	0.548	0.540	0.531	0.523	0.515	0.507	0.509	0.581	0.509	0.558	0.545	0.542	0.535	0.529	0.523	0.517	0.511	0.505	0.499	0.494	0.488	0.483										
45	0.562	0.554	0.545	0.537	0.529	0.521	0.513	0.505	0.500	0.549	0.536	0.533	0.526	0.520	0.514	0.508	0.502	0.496	0.491	0.485	0.480	0.474										
46	0.575	0.567	0.558	0.550	0.542	0.534	0.526	0.518	0.510	0.500	0.549	0.536	0.533	0.526	0.520	0.514	0.508	0.502	0.496	0.491	0.485	0.480										
47	0.589	0.581	0.572	0.564	0.556	0.548	0.540	0.532	0.524	0.516	0.506	0.500	0.493	0.487	0.481	0.475	0.469	0.463	0.457	0.452	0.446	0.440										
48	0.602	0.594	0.585	0.577	0.569	0.561	0.553	0.545	0.537	0.529	0.521	0.513	0.506	0.499	0.493	0.487	0.481	0.475	0.469	0.463	0.457	0.452										
49	0.615	0.607	0.598	0.590	0.582	0.574	0.566	0.558	0.550	0.542	0.534	0.526	0.519	0.512	0.506	0.500	0.494	0.488	0.482	0.476	0.470	0.465										
50	0.628	0.620	0.611	0.603	0.595	0.587	0.579	0.571	0.563	0.555	0.547	0.539	0.532	0.524	0.517	0.510	0.503	0.497	0.491	0.485	0.479	0.474										
51	0.641	0.633	0.624	0.616	0.608	0.600	0.592	0.584	0.576	0.568	0.560	0.552	0.544	0.536	0.528	0.521	0.513	0.506	0.500	0.494	0.488	0.483										
52	0.654	0.646	0.637	0.629	0.621	0.613	0.605	0.597	0.589	0.581	0.573	0.565	0.557	0.549	0.541	0.533	0.525	0.517	0.510	0.503	0.497	0.492										
53	0.667	0.659	0.650	0.642	0.634	0.626	0.618	0.610	0.602	0.594	0.586	0.578	0.570	0.562	0.554	0.546	0.538	0.530	0.522	0.514	0.506	0.500										
54	0.680	0.672	0.663	0.655	0.647	0.639	0.631	0.623	0.615	0.607	0.599	0.591	0.583	0.575	0.567	0.559	0.551	0.543	0.535	0.527	0.519	0.513										
55	0.693	0.685	0.676	0.668	0.660	0.652	0.644	0.636	0.628	0.620	0.612	0.604	0.596	0.588	0.580	0.572	0.564	0.556	0.548	0.540	0.532	0.526										
56	0.706	0.698	0.689	0.681	0.673	0.665	0.657	0.649	0.641	0.633	0.625	0.617	0.609	0.601	0.593	0.585	0.577	0.569	0.561	0.553	0.545	0.539										
57	0.719	0.711	0.702	0.694	0.686	0.678	0.670	0.662	0.654	0.646	0.638	0.630	0.622	0.614	0.606	0.598	0.590	0.582	0.574	0.566	0.558	0.552										
58	0.732	0.724	0.715	0.707	0.699	0.691	0.683	0.675	0.667	0.659	0.651	0.643	0.635	0.627	0.619	0.611	0.603	0.595	0.587	0.579	0.571	0.565										
59	0.745	0.737	0.728	0.720	0.712	0.704	0.696	0.688	0.680	0.672	0.664	0.656	0.648	0.640	0.632	0.624	0.616	0.608	0.600	0.592	0.584	0.578										
60	0.758	0.750	0.741	0.733	0.725	0.717	0.709	0.701	0.693	0.685	0.677	0.669	0.661	0.653	0.645	0.637	0.629	0.621	0.613	0.605	0.597	0.591										
61	0.771	0.763	0.754	0.746	0.738	0.730	0.722	0.714	0.706	0.698	0.690	0.682	0.674	0.666	0.658	0.650	0.642	0.634	0.626	0.618	0.610	0.604										
62	0.784	0.776	0.767	0.759	0.751	0.743	0.735	0.727	0.719	0.711	0.703	0.695	0.687	0.679	0.671	0.663	0.655	0.647	0.639	0.631	0.623	0.617										
63	0.797	0.789	0.780	0.772	0.764	0.756	0.748	0.740	0.732	0.724	0.716	0.708	0.700	0.692	0.684	0.676	0.668	0.660	0.652	0.644	0.636	0.630										
64	0.810	0.802	0.793	0.785	0.777	0.769	0.761	0.753	0.745	0.737	0.729	0.721	0.713	0.705	0.697	0.689	0.681	0.673	0.665	0.657	0.649	0.643										
65	0.823	0.815	0.806	0.798	0.790	0.782	0.774	0.766	0.758	0.750	0.742	0.734	0.726	0.718	0.710	0.702	0.694	0.686	0.678	0.670	0.662	0.656										
66	0.836	0.828	0.819	0.811	0.803	0.795	0.787	0.779	0.771	0.763	0.755	0.747	0.739	0.731	0.723	0.715	0.707	0.699	0.691	0.683	0.675	0.669										
67	0.849	0.841	0.832	0.824	0.816	0.808	0.800	0.792	0.784	0.776	0.768	0.760	0.752	0.744	0.736	0.728	0.720	0.712	0.704	0.696	0.688	0.682										
68	0.862	0.854	0.845	0.837	0.829	0.821	0.813	0.805	0.797	0.789	0.781	0.773	0.765	0.757	0.749	0.741	0.733	0.725	0.717	0.709	0.701	0.695										
69	0.875	0.867	0.858	0.850	0.842	0.834	0.826	0.818	0.810	0.802	0.794	0.786	0.778	0.770	0.762	0.754	0.746	0.738	0.730	0.722	0.714	0.708										
70	0.888	0.880	0.871	0.863	0.855	0.847	0.839	0.831	0.823	0.815	0.807	0.799	0.791	0.783	0.775	0.767	0.759	0.751	0.743	0.735	0.727	0.721										
71	0.901	0.893	0.884	0.876	0.868	0.860	0.852	0.844	0.836	0.828	0.820	0.812	0.804	0.796	0.788	0.780	0.772	0.764	0.756	0.748	0.740	0.734										
72	0.914	0.906	0.897	0.889	0.881	0.873	0.865	0.857	0.849	0.841	0.833	0.825	0.817	0.809	0.801	0.793	0.785	0.777	0.769	0.761	0.753	0.747										
73	0.927	0.919	0.910	0.902	0.894	0.886	0.878	0.870	0.862	0.854	0.846	0.838	0.830	0.822	0.814	0.806	0.798	0.790	0.782	0.774	0.766	0.760										
74	0.940	0.932	0.923	0.915	0.907	0.899	0.891	0.883	0.875	0.867	0.859	0.851	0.843	0.835	0.827	0.819	0.811	0.803	0.795	0.787	0.779	0.773										
75	0.953	0.945	0.936	0.928	0.920	0.912	0.904	0.896	0.888	0.880	0.872	0.864	0.856	0.848	0.840	0.832	0.824	0.816	0.808	0.800	0.792	0.786										
76	0.966	0.958	0.949	0.941	0.933	0.925	0.917	0.909	0.901	0.893	0.885	0.877	0.869	0.861	0.853	0.845	0.837	0.829	0.821	0.813	0.805	0.799										
77	0.979	0.971	0.962	0.954	0.946	0.938	0.930	0.922	0.914	0.906	0.898	0.890	0.882	0.874	0.866	0.858	0.850	0.842	0.834	0.826	0.818	0.812										
78	0.992	0.984	0.975	0.967	0.959	0.951	0.943	0.935	0.927	0.919	0.911	0.903	0.895	0.887	0.879	0.871	0.863	0.855	0.847	0.839	0.831	0.825										
79	1.005	0.997	0.988	0.980	0.972	0.964	0.956	0.948	0.940	0.932	0.924	0.916	0.908	0.900	0.892	0.884	0.876	0.868	0.860	0.852	0.844	0.838										
80	1.018	1.010	1.001	0.993	0.985	0.977	0.969	0.961	0.953	0.945	0.937	0.929	0.921	0.913	0.905	0.897	0.889	0.881	0.873	0.865	0.857	0.851										
81	1.031	1.023	1.014	1.006	0.998	0.990	0.982	0.974	0.966	0.958	0.950	0.942	0.934	0.926	0.918	0.910	0.902	0.894	0.886	0.878	0.870	0.864										
82	1.044	1.036	1.027	1.019	1.011	1.003	0.995	0.987	0.979	0.971	0.963	0.955	0.947	0.939	0.931	0.923	0.915	0.907	0.899	0.891	0.883	0.877										
83	1.057	1.049	1.040	1.032	1.024	1.016	1.008	1.000	0.992	0.984	0.976	0.968	0.960	0.952	0.944	0.936	0.928	0.920	0.912	0.904	0.896	0.890										
84	1.070	1.062	1.053	1.045	1.037	1.029	1.021	1.013	1.005	0.997	0.989	0.981	0.973	0.965	0.957	0.949	0.941	0.933	0.925	0.917	0.909	0.903										
85	1.083	1.075	1.066	1.058	1.050	1.042	1.034	1.026	1.018	1.010	1.002	0.994	0.986	0.978	0.970	0.962	0.954	0.946	0.938	0.930	0.922	0.916										
86	1.096	1.088	1.079	1.071	1.063	1.055	1.047	1.039	1.031	1.023	1.015	1.007	0.999	0.991	0.983	0.975	0.967	0.959	0.951	0.943	0.935	0.929										
87	1.109	1.101	1.092	1.084	1.076	1.068	1.060	1.052	1.044	1.036	1.028	1.020	1.012	1.004	0.996	0.988	0.980	0.972	0.964	0.956	0.948	0.942										
88	1.122	1.114	1.105	1.097	1.089	1.081	1.073	1.065	1.057	1.049	1.041	1.033	1.025	1.017	1.009	1.001	0.993	0.985	0.977	0.969	0.961	0.955										
89	1.135	1.127	1.118	1.110	1.102	1.094	1.086	1.078	1.070	1.062	1.054	1.046	1.038	1.030	1.022	1.014	1.006	0.998	0.990	0.982	0.974	0.968										
90	1.148	1.140	1.131	1.123	1.115	1.107	1.099	1.091	1.083	1.075	1.067	1.059	1.051	1.043	1.035	1.027	1.019	1.011	1.003	0.9												

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Fig. 10d

mCi per cGy matrix

Total Dose Lean Dose	V	T-1/2(T _{eff}) effective →										A0 (mCi/cGy)			
		83	84	85	86	87	88	89	90	91	92	93	94	95	96
40	0.481	0.456	0.431	0.406	0.381	0.356	0.331	0.306	0.281	0.256	0.231	0.206	0.181	0.156	0.131
41	0.471	0.446	0.421	0.396	0.371	0.346	0.321	0.296	0.271	0.246	0.221	0.196	0.171	0.146	0.121
42	0.462	0.437	0.412	0.387	0.362	0.337	0.312	0.287	0.262	0.237	0.212	0.187	0.162	0.137	0.112
43	0.452	0.427	0.402	0.377	0.352	0.327	0.302	0.277	0.252	0.227	0.202	0.177	0.152	0.127	0.102
44	0.442	0.417	0.392	0.367	0.342	0.317	0.292	0.267	0.242	0.217	0.192	0.167	0.142	0.117	0.092
45	0.432	0.407	0.382	0.357	0.332	0.307	0.282	0.257	0.232	0.207	0.182	0.157	0.132	0.107	0.082
46	0.422	0.397	0.372	0.347	0.322	0.297	0.272	0.247	0.222	0.197	0.172	0.147	0.122	0.097	0.072
47	0.412	0.387	0.362	0.337	0.312	0.287	0.262	0.237	0.212	0.187	0.162	0.137	0.112	0.087	0.062
48	0.402	0.377	0.352	0.327	0.302	0.277	0.252	0.227	0.202	0.177	0.152	0.127	0.102	0.077	0.052
49	0.392	0.367	0.342	0.317	0.292	0.267	0.242	0.217	0.192	0.167	0.142	0.117	0.092	0.067	0.042
50	0.382	0.357	0.332	0.307	0.282	0.257	0.232	0.207	0.182	0.157	0.132	0.107	0.082	0.057	0.032
51	0.372	0.347	0.322	0.297	0.272	0.247	0.222	0.197	0.172	0.147	0.122	0.097	0.072	0.047	0.022
52	0.362	0.337	0.312	0.287	0.262	0.237	0.212	0.187	0.162	0.137	0.112	0.087	0.062	0.037	0.012
53	0.352	0.327	0.302	0.277	0.252	0.227	0.202	0.177	0.152	0.127	0.102	0.077	0.052	0.027	0.002
54	0.342	0.317	0.292	0.267	0.242	0.217	0.192	0.167	0.142	0.117	0.092	0.067	0.042	0.017	0.002
55	0.332	0.307	0.282	0.257	0.232	0.207	0.182	0.157	0.132	0.107	0.082	0.057	0.032	0.007	0.002
56	0.322	0.297	0.272	0.247	0.222	0.197	0.172	0.147	0.122	0.097	0.072	0.047	0.022	0.007	0.002
57	0.312	0.287	0.262	0.237	0.212	0.187	0.162	0.137	0.112	0.087	0.062	0.037	0.012	0.007	0.002
58	0.302	0.277	0.252	0.227	0.202	0.177	0.152	0.127	0.102	0.077	0.052	0.027	0.007	0.002	0.002
59	0.292	0.267	0.242	0.217	0.192	0.167	0.142	0.117	0.092	0.067	0.042	0.017	0.007	0.002	0.002
60	0.282	0.257	0.232	0.207	0.182	0.157	0.132	0.107	0.082	0.057	0.032	0.007	0.002	0.002	0.002
61	0.272	0.247	0.222	0.197	0.172	0.147	0.122	0.097	0.072	0.047	0.022	0.007	0.002	0.002	0.002
62	0.262	0.237	0.212	0.187	0.162	0.137	0.112	0.087	0.062	0.037	0.012	0.007	0.002	0.002	0.002
63	0.252	0.227	0.202	0.177	0.152	0.127	0.102	0.077	0.052	0.027	0.007	0.002	0.002	0.002	0.002
64	0.242	0.217	0.192	0.167	0.142	0.117	0.092	0.067	0.042	0.017	0.007	0.002	0.002	0.002	0.002
65	0.232	0.207	0.182	0.157	0.132	0.107	0.082	0.057	0.032	0.007	0.002	0.002	0.002	0.002	0.002
66	0.222	0.197	0.172	0.147	0.122	0.097	0.072	0.047	0.022	0.007	0.002	0.002	0.002	0.002	0.002
67	0.212	0.187	0.162	0.137	0.112	0.087	0.062	0.037	0.012	0.007	0.002	0.002	0.002	0.002	0.002
68	0.202	0.177	0.152	0.127	0.102	0.077	0.052	0.027	0.007	0.002	0.002	0.002	0.002	0.002	0.002
69	0.192	0.167	0.142	0.117	0.092	0.067	0.042	0.017	0.007	0.002	0.002	0.002	0.002	0.002	0.002
70	0.182	0.157	0.132	0.107	0.082	0.057	0.032	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002
71	0.172	0.147	0.122	0.097	0.072	0.047	0.022	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002
72	0.162	0.137	0.112	0.087	0.062	0.037	0.012	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002
73	0.152	0.127	0.102	0.077	0.052	0.027	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
74	0.142	0.117	0.092	0.067	0.042	0.017	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
75	0.132	0.107	0.082	0.057	0.032	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
76	0.122	0.097	0.072	0.047	0.022	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
77	0.112	0.087	0.062	0.037	0.012	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
78	0.102	0.077	0.052	0.027	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
79	0.092	0.067	0.042	0.017	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
80	0.082	0.057	0.032	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
81	0.072	0.047	0.022	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
82	0.062	0.037	0.012	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002
83	0.052	0.027	0.007	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.002

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Fig. 10e

mCi per cGy matrix

Activity per unit Total Body Dose (TBD) or Lean Body Dose (LBD-Lean) as a function of Total Body or Lean body mass and T1/2-effective

LBD estimates from:

Female: $LBD = 48.5 \div 0.81 \cdot (HT - 152)$ [HT in cm, LBD in Kg]Male: $LBD = 48.0 \div 1.06 \cdot (HT - 152)$ Total Body mass for Total Body dose
Lean Body mass (LBD) for Total Body Dose-Lean

V	T1/2-effective -->	30	31	32	33	34	35	36	37	38	39	40	41	42	43	44	45	46	47	48	49	50
84	2.790	2.700	2.610	2.520	2.430	2.340	2.250	2.160	2.070	1.980	1.890	1.800	1.710	1.620	1.530	1.440	1.350	1.260	1.170	1.080	1.000	1.000
85	2.820	2.720	2.630	2.540	2.450	2.360	2.270	2.180	2.090	2.000	1.910	1.820	1.730	1.640	1.550	1.460	1.370	1.280	1.190	1.100	1.020	1.020
86	2.840	2.740	2.650	2.560	2.470	2.380	2.290	2.200	2.110	2.020	1.930	1.840	1.750	1.660	1.570	1.480	1.390	1.300	1.210	1.120	1.040	1.040
87	2.870	2.770	2.680	2.590	2.500	2.410	2.320	2.230	2.140	2.050	1.960	1.870	1.780	1.690	1.600	1.510	1.420	1.330	1.240	1.150	1.070	1.070
88	2.900	2.800	2.710	2.620	2.530	2.440	2.350	2.260	2.170	2.080	1.990	1.900	1.810	1.720	1.630	1.540	1.450	1.360	1.270	1.180	1.100	1.100
89	2.930	2.830	2.740	2.650	2.560	2.470	2.380	2.290	2.200	2.110	2.020	1.930	1.840	1.750	1.660	1.570	1.480	1.390	1.300	1.210	1.130	1.130
90	2.960	2.860	2.770	2.680	2.590	2.500	2.410	2.320	2.230	2.140	2.050	1.960	1.870	1.780	1.690	1.600	1.510	1.420	1.330	1.240	1.160	1.160
91	2.990	2.890	2.800	2.710	2.620	2.530	2.440	2.350	2.260	2.170	2.080	1.990	1.900	1.810	1.720	1.630	1.540	1.450	1.360	1.270	1.190	1.190
92	3.020	2.920	2.830	2.740	2.650	2.560	2.470	2.380	2.290	2.200	2.110	2.020	1.930	1.840	1.750	1.660	1.570	1.480	1.390	1.300	1.220	1.220
93	3.050	2.950	2.860	2.770	2.680	2.590	2.500	2.410	2.320	2.230	2.140	2.050	1.960	1.870	1.780	1.690	1.600	1.510	1.420	1.330	1.250	1.250
94	3.080	2.980	2.890	2.800	2.710	2.620	2.530	2.440	2.350	2.260	2.170	2.080	1.990	1.900	1.810	1.720	1.630	1.540	1.450	1.360	1.280	1.280
95	3.110	3.010	2.920	2.830	2.740	2.650	2.560	2.470	2.380	2.290	2.200	2.110	2.020	1.930	1.840	1.750	1.660	1.570	1.480	1.390	1.310	1.310
96	3.140	3.040	2.950	2.860	2.770	2.680	2.590	2.500	2.410	2.320	2.230	2.140	2.050	1.960	1.870	1.780	1.690	1.600	1.510	1.420	1.340	1.340
97	3.170	3.070	2.980	2.890	2.800	2.710	2.620	2.530	2.440	2.350	2.260	2.170	2.080	1.990	1.900	1.810	1.720	1.630	1.540	1.450	1.370	1.370
98	3.200	3.100	3.000	2.910	2.820	2.730	2.640	2.550	2.460	2.370	2.280	2.190	2.100	2.010	1.920	1.830	1.740	1.650	1.560	1.470	1.390	1.390
99	3.230	3.130	3.030	2.940	2.850	2.760	2.670	2.580	2.490	2.400	2.310	2.220	2.130	2.040	1.950	1.860	1.770	1.680	1.590	1.500	1.420	1.420
100	3.260	3.160	3.060	2.970	2.880	2.790	2.700	2.610	2.520	2.430	2.340	2.250	2.160	2.070	1.980	1.890	1.800	1.710	1.620	1.530	1.450	1.450
101	3.290	3.190	3.090	2.990	2.900	2.810	2.720	2.630	2.540	2.450	2.360	2.270	2.180	2.090	2.000	1.910	1.820	1.730	1.640	1.550	1.470	1.470
102	3.320	3.210	3.110	3.020	2.930	2.840	2.750	2.660	2.570	2.480	2.390	2.300	2.210	2.120	2.030	1.940	1.850	1.760	1.670	1.580	1.500	1.500
103	3.350	3.240	3.140	3.050	2.960	2.870	2.780	2.690	2.600	2.510	2.420	2.330	2.240	2.150	2.060	1.970	1.880	1.790	1.700	1.610	1.530	1.530
104	3.380	3.270	3.170	3.080	2.990	2.900	2.810	2.720	2.630	2.540	2.450	2.360	2.270	2.180	2.090	2.000	1.910	1.820	1.730	1.640	1.560	1.560
105	3.410	3.300	3.190	3.100	3.000	2.910	2.820	2.730	2.640	2.550	2.460	2.370	2.280	2.190	2.100	2.010	1.920	1.830	1.740	1.650	1.570	1.570
106	3.430	3.320	3.220	3.120	3.030	2.940	2.850	2.760	2.670	2.580	2.490	2.400	2.310	2.220	2.130	2.040	1.950	1.860	1.770	1.680	1.600	1.600
107	3.460	3.350	3.250	3.150	3.060	2.970	2.880	2.790	2.700	2.610	2.520	2.430	2.340	2.250	2.160	2.070	1.980	1.890	1.800	1.710	1.630	1.630
108	3.490	3.380	3.280	3.180	3.090	2.990	2.900	2.810	2.720	2.630	2.540	2.450	2.360	2.270	2.180	2.090	2.000	1.910	1.820	1.730	1.650	1.650
109	3.520	3.410	3.300	3.200	3.110	3.020	2.930	2.840	2.750	2.660	2.570	2.480	2.390	2.300	2.210	2.120	2.030	1.940	1.850	1.760	1.680	1.680
110	3.550	3.440	3.330	3.230	3.140	3.050	2.960	2.870	2.780	2.690	2.600	2.510	2.420	2.330	2.240	2.150	2.060	1.970	1.880	1.790	1.710	1.710
111	3.580	3.470	3.360	3.260	3.170	3.080	2.990	2.900	2.810	2.720	2.630	2.540	2.450	2.360	2.270	2.180	2.090	2.000	1.910	1.820	1.740	1.740
112	3.610	3.500	3.390	3.290	3.190	3.100	3.010	2.920	2.830	2.740	2.650	2.560	2.470	2.380	2.290	2.200	2.110	2.020	1.930	1.840	1.760	1.760
113	3.640	3.530	3.420	3.320	3.220	3.130	3.040	2.950	2.860	2.770	2.680	2.590	2.500	2.410	2.320	2.230	2.140	2.050	1.960	1.870	1.790	1.790
114	3.670	3.560	3.450	3.350	3.250	3.160	3.070	2.980	2.890	2.800	2.710	2.620	2.530	2.440	2.350	2.260	2.170	2.080	1.990	1.900	1.820	1.820
115	3.690	3.580	3.470	3.370	3.270	3.180	3.090	3.000	2.910	2.820	2.730	2.640	2.550	2.460	2.370	2.280	2.190	2.100	2.010	1.920	1.840	1.840
116	3.720	3.600	3.490	3.390	3.290	3.190	3.100	3.010	2.920	2.830	2.740	2.650	2.560	2.470	2.380	2.290	2.200	2.110	2.020	1.930	1.850	1.850
117	3.750	3.630	3.520	3.420	3.320	3.220	3.130	3.040	2.950	2.860	2.770	2.680	2.590	2.500	2.410	2.320	2.230	2.140	2.050	1.960	1.880	1.880
118	3.780	3.660	3.550	3.450	3.350	3.250	3.160	3.070	2.980	2.890	2.800	2.710	2.620	2.530	2.440	2.350	2.260	2.170	2.080	1.990	1.910	1.910
119	3.810	3.690	3.580	3.480	3.380	3.280	3.190	3.100	3.010	2.920	2.830	2.740	2.650	2.560	2.470	2.380	2.290	2.200	2.110	2.020	1.940	1.940
120	3.840	3.710	3.600	3.490	3.390	3.290	3.190	3.100	3.010	2.920	2.830	2.740	2.650	2.560	2.470	2.380	2.290	2.200	2.110	2.020	1.940	1.940

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Fig. 10f

mCi per cdy matrix

Total Bod Lean Bod	V	1-1/2 hr effective →	51	52	53	54	55	56	57	58	59	60	61	62	63	64	65	66	67	68	69	70	71
			1.941	1.910	1.879	1.850	1.822	1.795	1.768	1.743	1.718	1.695	1.672	1.650	1.629	1.608	1.588	1.568	1.548	1.528	1.508	1.488	1.468
			1.959	1.927	1.896	1.866	1.836	1.811	1.784	1.759	1.734	1.709	1.684	1.659	1.634	1.609	1.584	1.559	1.534	1.509	1.484	1.459	1.434
			1.978	1.944	1.913	1.883	1.854	1.826	1.798	1.771	1.744	1.717	1.690	1.663	1.636	1.609	1.582	1.555	1.528	1.501	1.474	1.447	1.420
			1.993	1.961	1.930	1.899	1.870	1.842	1.814	1.786	1.758	1.730	1.702	1.674	1.646	1.618	1.590	1.562	1.534	1.506	1.478	1.450	1.422
			1.711	1.676	1.646	1.616	1.586	1.556	1.531	1.504	1.478	1.451	1.424	1.397	1.370	1.343	1.316	1.289	1.262	1.235	1.208	1.181	1.154
			1.728	1.695	1.665	1.635	1.605	1.575	1.548	1.520	1.494	1.467	1.440	1.413	1.386	1.359	1.332	1.305	1.278	1.251	1.224	1.197	1.170
			1.748	1.712	1.682	1.652	1.622	1.592	1.565	1.538	1.511	1.484	1.457	1.430	1.403	1.376	1.349	1.322	1.295	1.268	1.241	1.214	1.187
			1.763	1.729	1.697	1.666	1.635	1.606	1.578	1.550	1.524	1.498	1.471	1.444	1.417	1.390	1.363	1.336	1.309	1.282	1.255	1.228	1.201
			1.781	1.746	1.713	1.682	1.651	1.622	1.593	1.568	1.541	1.514	1.487	1.460	1.433	1.406	1.379	1.352	1.325	1.298	1.271	1.244	1.217
			1.798	1.763	1.730	1.698	1.667	1.638	1.608	1.581	1.554	1.528	1.501	1.474	1.447	1.420	1.393	1.366	1.339	1.312	1.285	1.258	1.231
			1.815	1.781	1.747	1.716	1.683	1.653	1.624	1.598	1.569	1.543	1.516	1.489	1.462	1.435	1.408	1.381	1.354	1.327	1.300	1.273	1.246
			1.833	1.798	1.764	1.731	1.700	1.669	1.640	1.612	1.584	1.556	1.528	1.500	1.472	1.444	1.416	1.388	1.360	1.332	1.304	1.276	1.248
			1.850	1.815	1.781	1.748	1.716	1.685	1.656	1.627	1.598	1.573	1.547	1.522	1.496	1.470	1.444	1.418	1.392	1.366	1.340	1.314	1.288
			1.868	1.832	1.797	1.764	1.732	1.701	1.671	1.642	1.615	1.588	1.562	1.536	1.510	1.484	1.458	1.432	1.406	1.380	1.354	1.328	1.302
			1.885	1.848	1.814	1.780	1.748	1.717	1.687	1.658	1.630	1.602	1.576	1.551	1.526	1.501	1.475	1.449	1.423	1.397	1.371	1.345	1.319
			1.903	1.866	1.831	1.797	1.764	1.733	1.702	1.673	1.645	1.617	1.591	1.565	1.540	1.514	1.488	1.462	1.436	1.410	1.384	1.358	1.332
			1.920	1.883	1.847	1.813	1.780	1.748	1.716	1.686	1.656	1.628	1.601	1.574	1.548	1.522	1.496	1.470	1.444	1.418	1.392	1.366	1.340
			1.937	1.900	1.864	1.830	1.796	1.764	1.733	1.703	1.675	1.647	1.620	1.594	1.568	1.542	1.516	1.490	1.464	1.438	1.412	1.386	1.360
			1.954	1.917	1.881	1.848	1.812	1.780	1.748	1.719	1.689	1.661	1.634	1.608	1.582	1.557	1.532	1.507	1.481	1.455	1.429	1.403	1.377
			1.972	1.934	1.897	1.862	1.828	1.796	1.764	1.734	1.704	1.676	1.649	1.622	1.596	1.571	1.547	1.524	1.501	1.477	1.453	1.429	1.405
			1.988	1.951	1.914	1.878	1.844	1.811	1.779	1.748	1.718	1.689	1.661	1.634	1.608	1.583	1.559	1.535	1.511	1.487	1.463	1.439	1.415
			2.006	1.967	1.930	1.894	1.860	1.827	1.795	1.764	1.734	1.705	1.677	1.650	1.624	1.599	1.574	1.550	1.527	1.504	1.481	1.458	1.435
			2.023	1.984	1.947	1.911	1.878	1.842	1.810	1.778	1.748	1.720	1.691	1.664	1.638	1.612	1.587	1.563	1.540	1.517	1.494	1.471	1.448
			2.040	2.001	1.963	1.927	1.893	1.859	1.825	1.794	1.763	1.734	1.706	1.678	1.651	1.625	1.601	1.577	1.553	1.530	1.508	1.485	1.463
			2.057	2.017	1.979	1.943	1.907	1.873	1.840	1.808	1.778	1.748	1.720	1.692	1.665	1.639	1.614	1.589	1.565	1.542	1.519	1.496	1.473
			2.074	2.034	1.998	1.962	1.926	1.892	1.858	1.826	1.795	1.765	1.735	1.706	1.678	1.652	1.627	1.603	1.579	1.555	1.532	1.509	1.486
			2.091	2.051	2.012	1.975	1.939	1.904	1.871	1.838	1.807	1.777	1.747	1.720	1.693	1.668	1.644	1.620	1.597	1.574	1.551	1.528	1.505
			2.108	2.067	2.028	1.991	1.954	1.920	1.886	1.853	1.822	1.792	1.762	1.734	1.706	1.680	1.654	1.629	1.604	1.581	1.558	1.535	1.512
			2.125	2.084	2.044	2.007	1.970	1.935	1.901	1.868	1.837	1.807	1.777	1.748	1.720	1.694	1.668	1.643	1.619	1.595	1.572	1.549	1.526
			2.141	2.100	2.061	2.022	1.986	1.950	1.916	1.883	1.851	1.820	1.790	1.761	1.734	1.708	1.682	1.657	1.633	1.609	1.585	1.562	1.539
			2.158	2.117	2.077	2.038	2.001	1.968	1.934	1.901	1.868	1.837	1.807	1.778	1.751	1.724	1.700	1.675	1.651	1.627	1.603	1.579	1.555
			2.175	2.133	2.093	2.054	2.017	1.981	1.946	1.913	1.880	1.849	1.819	1.789	1.761	1.734	1.709	1.684	1.660	1.636	1.612	1.588	1.564
			2.192	2.150	2.109	2.070	2.032	1.996	1.961	1.927	1.895	1.863	1.832	1.803	1.774	1.747	1.722	1.697	1.673	1.649	1.625	1.601	1.577
			2.209	2.168	2.126	2.088	2.049	2.012	1.976	1.941	1.908	1.876	1.845	1.814	1.786	1.759	1.734	1.709	1.685	1.661	1.637	1.613	1.589
			2.226	2.182	2.141	2.102	2.063	2.027	1.991	1.957	1.923	1.891	1.860	1.830	1.801	1.774	1.749	1.724	1.700	1.676	1.652	1.628	1.604
			2.242	2.199	2.157	2.117	2.078	2.042	2.006	1.971	1.938	1.906	1.874	1.844	1.815	1.787	1.761	1.736	1.711	1.687	1.663	1.639	1.615
			2.259	2.215	2.173	2.133	2.094	2.057	2.021	1.986	1.952	1.920	1.888	1.857	1.828	1.800	1.774	1.749	1.724	1.700	1.676	1.652	1.628

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Fig. 10h

mCi per cOy matrix

Total Bod Lean Bod	V	T-1/2(h)-effective -->					A0 (mCi-cOy)				
		92	94	96	98	100	92	94	96	98	100
94	0.900	0.900	0.901	0.902	0.903	0.904	0.905	0.906	0.907	0.908	0.909
95	0.910	0.910	0.911	0.912	0.913	0.914	0.915	0.916	0.917	0.918	0.919
96	0.920	0.920	0.921	0.922	0.923	0.924	0.925	0.926	0.927	0.928	0.929
97	0.930	0.930	0.931	0.932	0.933	0.934	0.935	0.936	0.937	0.938	0.939
98	0.940	0.940	0.941	0.942	0.943	0.944	0.945	0.946	0.947	0.948	0.949
99	0.950	0.950	0.951	0.952	0.953	0.954	0.955	0.956	0.957	0.958	0.959
100	0.960	0.960	0.961	0.962	0.963	0.964	0.965	0.966	0.967	0.968	0.969
101	0.970	0.970	0.971	0.972	0.973	0.974	0.975	0.976	0.977	0.978	0.979
102	0.980	0.980	0.981	0.982	0.983	0.984	0.985	0.986	0.987	0.988	0.989
103	0.990	0.990	0.991	0.992	0.993	0.994	0.995	0.996	0.997	0.998	0.999
104	1.000	1.000	1.001	1.002	1.003	1.004	1.005	1.006	1.007	1.008	1.009
105	1.010	1.010	1.011	1.012	1.013	1.014	1.015	1.016	1.017	1.018	1.019
106	1.020	1.020	1.021	1.022	1.023	1.024	1.025	1.026	1.027	1.028	1.029
107	1.030	1.030	1.031	1.032	1.033	1.034	1.035	1.036	1.037	1.038	1.039
108	1.040	1.040	1.041	1.042	1.043	1.044	1.045	1.046	1.047	1.048	1.049
109	1.050	1.050	1.051	1.052	1.053	1.054	1.055	1.056	1.057	1.058	1.059
110	1.060	1.060	1.061	1.062	1.063	1.064	1.065	1.066	1.067	1.068	1.069
111	1.070	1.070	1.071	1.072	1.073	1.074	1.075	1.076	1.077	1.078	1.079
112	1.080	1.080	1.081	1.082	1.083	1.084	1.085	1.086	1.087	1.088	1.089
113	1.090	1.090	1.091	1.092	1.093	1.094	1.095	1.096	1.097	1.098	1.099
114	1.100	1.100	1.101	1.102	1.103	1.104	1.105	1.106	1.107	1.108	1.109
115	1.110	1.110	1.111	1.112	1.113	1.114	1.115	1.116	1.117	1.118	1.119
116	1.120	1.120	1.121	1.122	1.123	1.124	1.125	1.126	1.127	1.128	1.129
117	1.130	1.130	1.131	1.132	1.133	1.134	1.135	1.136	1.137	1.138	1.139
118	1.140	1.140	1.141	1.142	1.143	1.144	1.145	1.146	1.147	1.148	1.149
119	1.150	1.150	1.151	1.152	1.153	1.154	1.155	1.156	1.157	1.158	1.159
120	1.160	1.160	1.161	1.162	1.163	1.164	1.165	1.166	1.167	1.168	1.169

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3-D mCi per cGy

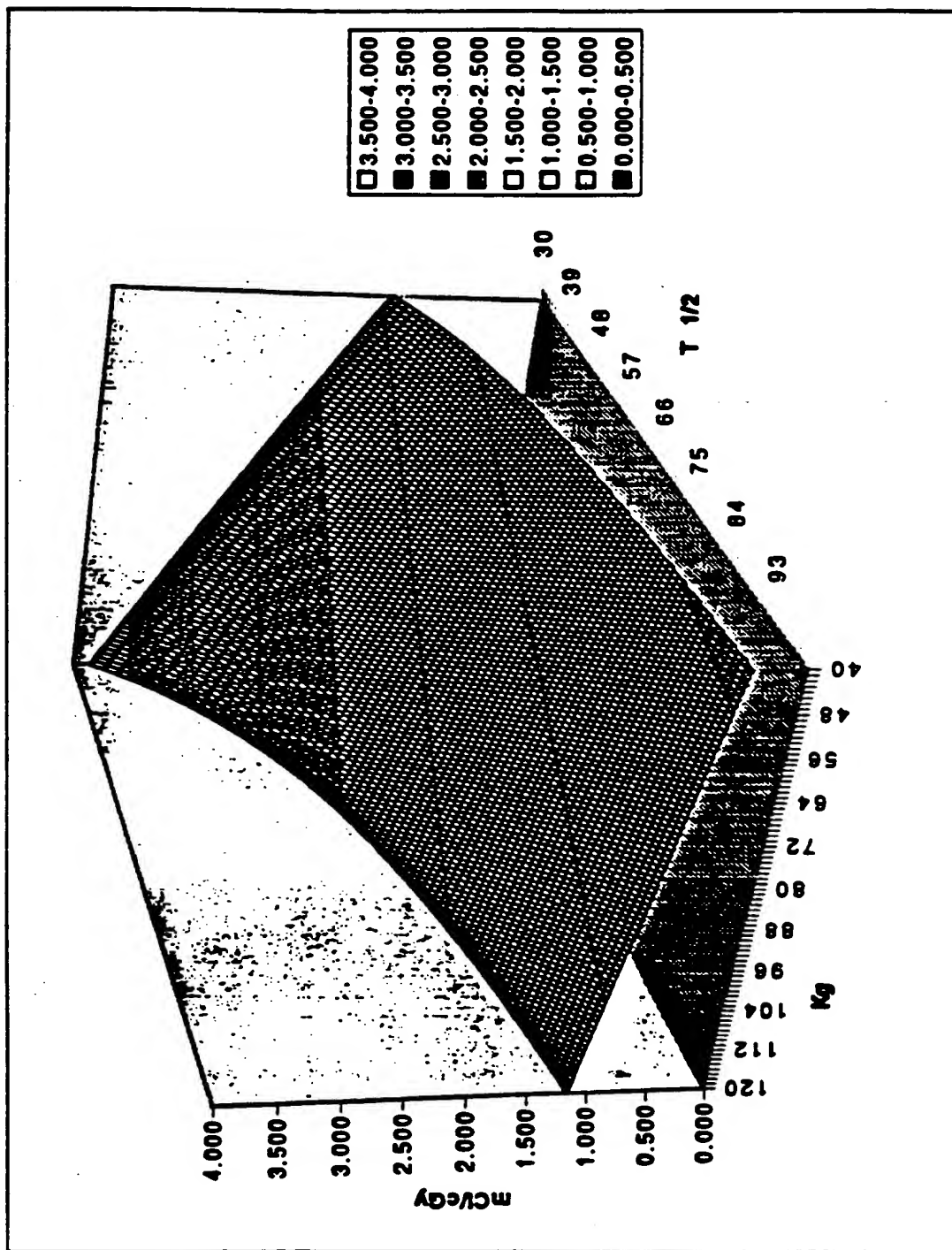


Fig. 11

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toxicity_noBMT.bt

pl num	mCi	TB-kg	TB-dose	Blood-dose	narrow-dose	LBM	tox-grade	mCiperKG	mCipermsq	mCiperLBM	TBLBmdose
1	66.0	72.8	25.0	126	51	74.606	1	0.907	34.8	0.885	25.8
2	45.1	77.2	25.0	141	55	69.2	0	0.584	23.7	0.652	28.2
4	57.0	80.8	25.0	166	64	66.974	1	0.705	29.6	0.851	31.4
5	38.0	74.9	35.0	186	76	74.924	1	0.507	19.8	0.507	33.6
6	40.0	81.3	35.0	257	99	81.39	1	0.492	19.6	0.491	34.6
7	41.0	82.6	35.0	126	60	81.602	0	0.496	20.0	0.502	37.6
8	39.8	84.2	35.0	146	67	71.002	2	0.473	20.0	0.561	42.4
9	43.5	86.0	45.0	269	104	54.042	0	0.659	26.0	0.805	55.9
10	61.5	90.0	45.0	291	118	77.68	0	0.683	29.3	0.792	52.2
13	40.5	60.5	45.0	293	112	55.965	0	0.669	24.5	0.724	50.7
14	68.3	83.3	55.0	305	127	73.334	0	0.820	34.2	0.931	64.3
15	44.1	54.4	55.0	265	105	58.24	3	0.811	27.6	0.757	53.7
16	70.9	93.4	55.0	381	153	73.97	2	0.759	33.7	0.958	70.1
19	68.5	82.3	65.0	370	158	56.602	1	0.832	36.2	1.210	92.2
24	106.7	83.1	75.0	340	148	83.934	0	1.284	51.4	1.271	71.4
27	97.9	73.0	85.0	443	187	57.785	0	1.341	54.2	1.694	108.5
28	95.6	86.4	85.0	228	121	79.164	4	1.106	46.1	1.208	97.5
29	161.0	136.0	85.0	474	241	70.343	4	1.184	64.5	2.289	164.4
31	107.5	91.8	75.0	232	120	70.578	3	1.171	52.2	1.523	108.4
32	56.8	48.0	75.0	457	169	47.32	0	1.183	39.6	1.200	80.0
34	102.5	88.6	75.0	517	205	78.74	2	1.157	49.0	1.302	82.6

Fig. 12

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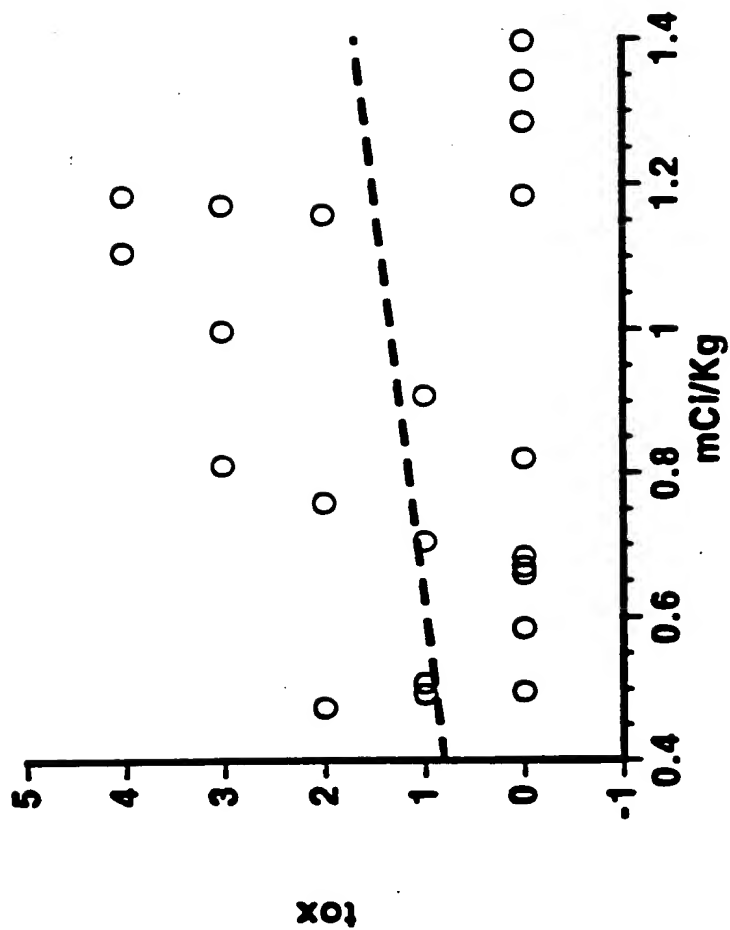
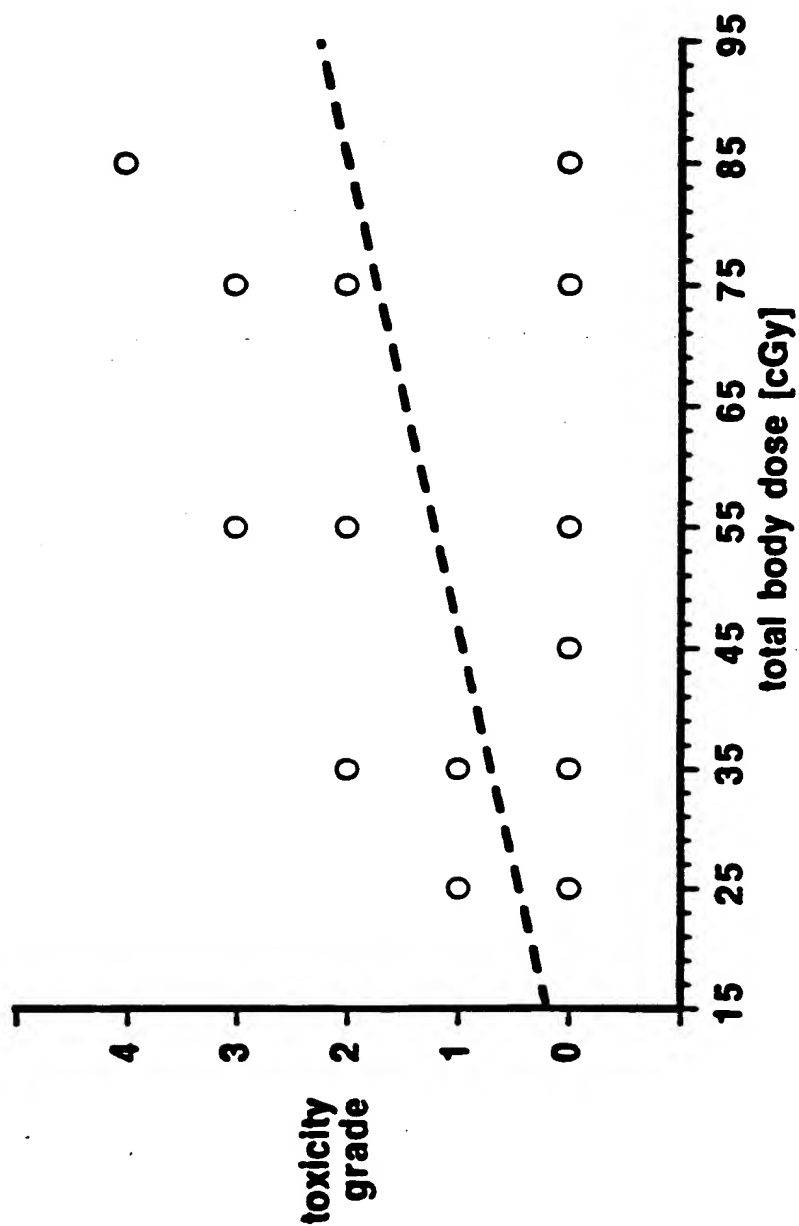
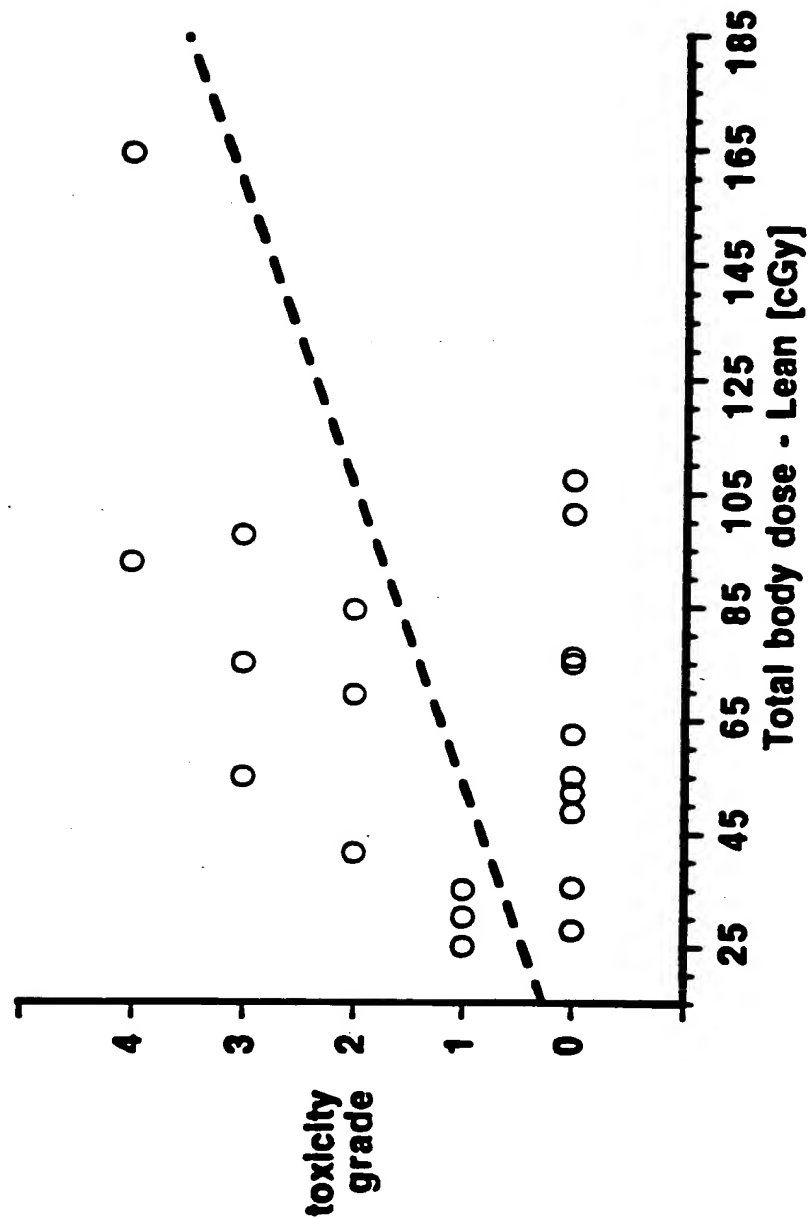
Fig. 13

Fig. 14

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Fig. 15

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US96/06240**A. CLASSIFICATION OF SUBJECT MATTER**

IPC(6) : A61K 51/00; A61B 6/00; A61F 5/00

US CL : 424/1.11, 1,65; 128/659; 604/20

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 424/1.11, 1,65; 128/659; 604/20

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

APS, MEDLINE, BIOSIS, SCISEARCH, WPIDS

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	ZASADNY et al. Standardized Uptake Values of Normal Tissues at PET with 2-[Fluorine-18]-Fluoro-2-deoxy-D-glucose: Variations with Body Weight and a Method for Correction. Radiology. 01 December 1993, Vol. 189, No. 3, pages 847-850.	1-25
Y	KORAL et al. CT-SPECT Fusion Plus Conjugate Views for Determining Dosimetry in Iodine-131-Monoclonal Antibody Therapy of Lymphoma Patients. The Journal of Nuclear Medicine. Vol. 35, No. 10, 01 October 1994, pages 1714-1720.	1-25

☒ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

•	Special categories of cited documents:	•T	later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
•A	document defining the general state of the art which is not considered to be of particular relevance		
•E	earlier document published on or after the international filing date	•X	document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
•L	document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	•Y	document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
•O	document referring to an oral disclosure, use, exhibition or other means		
•P	document published prior to the international filing date but later than the priority date claimed	•&	document member of the same patent family

Date of the actual completion of the international search

18 JULY 1996

Date of mailing of the international search report

11 SEP 1996

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INTERNATIONAL SEARCH REPORT

International application No.
PCT/US96/06240

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	KAMINSKY et al. Radioimmunotherapy of B-cell LYmphoma [I-131]Anti-B1 (Anti-CD20) Antibody. The New England Journal of Medicine, Vol. 329, No. 7, 12 August 1993, pages 459-465.	1-25